

Mechanically interlocked stretchable nanofibers for multifunctional wearable triboelectric nanogenerator

Li, Yi; Xiong, Jiaqing; Lv, Jian; Chen, Jian; Gao, Dace; Zhang, Xiaoxing; Lee, Pooi See

2020

Li, Y., Xiong, J., Lv, J., Chen, J., Gao, D., Zhang, X., & Lee, P. S. (2020). Mechanically interlocked stretchable nanofibers for multifunctional wearable triboelectric nanogenerator. *Nano Energy*, 78, 105358. doi:10.1016/j.nanoen.2020.105358

<https://hdl.handle.net/10356/143797>

<https://doi.org/10.1016/j.nanoen.2020.105358>

© 2020 Elsevier Ltd. All rights reserved. This paper was published in *Nano Energy* and is made available with permission of Elsevier Ltd.

Downloaded on 26 Mar 2023 05:25:44 SGT

1 Mechanically interlocked stretchable nanofibers for multifunctional 2 wearable triboelectric nanogenerator

3 Yi Li ^{1,2,#}, Jiaqing Xiong ^{1,#}, Jian Lv ¹, Jian Chen ¹, Dace Gao ¹, Xiaoxing Zhang ^{2,3*} and Pooi See
4 Lee ^{1,*}

5 ¹ School of Materials Science and Engineering, Nanyang Technological University, 50 Nanyang Avenue,
6 639798, Singapore

7 ² School of Electrical Engineering and Automation, Wuhan University, Wuhan, Hubei 430072, China

8 ³ Key Laboratory for High-Efficiency Utilization of Solar Energy and Operation Control of Energy Storage
9 System, School of Electrical and Electronic Engineering, Hubei University of Technology, Wuhan 430068,
10 China

11 #The authors contributed equally to this work.

12 *Corresponding author: pslee@ntu.edu.sg, xiaoxing.zhang@outlook.com

13 Abstract

14 Nanofibers with good softness and high surface specific area are excellent choices for wearable tribo-
15 electric nanogenerator (TENG), despite that the deformability and durability remain challenging in
16 seamless integration with daily textiles/clothes. Herein, we propose a physical interlocking strategy to re-
17 alize a self-interlocked stretchable, breathable and waterproof nanofibers-membrane by simultaneous
18 electrospinning of poly (vinylidene fluoride-co-hexafluoropropylene) (PVDF-HFP) and electrospaying of
19 styrene-ethylene-butylene-styrene (SEBS). The electrospayed SEBS microspheres serve as the elastic
20 binders and hydrophobic modifiers for enhancing stretchability and waterproofness of the electrospun
21 PVDF-HFP fibers network. By means of a printable electrode consisted of liquid metal (gallium indium tin
22 particles) and silver flakes, a stretchable nanofibers-based TENG (SNF-TENG) with high triboelectric
23 output (85 V, 219.66 mW m⁻²) and electrical durability was demonstrated, capable of harvesting energy
24 from human motions and flowing water, powering 200 commercial LEDs and an electronic watch. The
25 stretchable nanofibers membrane shows favorable mechanical compliance, which can be facilely integrat-
26 ed onto a stretchable textile to fabricate textile-TENG, promising for comfortable wearable applications for

1 power sources, smart raincoat, self-powered e-skin and tactile interactive interfaces.

2 **Key Words:** mechanically interlocked, stretchable nanofiber, breathable, waterproof, triboelectric nano-
3 generator, electronic skins

4 **1 Introduction**

5 Wearable electronic devices with light-weight, high performance and mechanical compliance are de-
6 sired for seamless integration with clothes and human body, realizing diverse applications encompassing
7 smart sensors, electronic skin (e-skin) and health-monitoring gadgets, which also motivated the develop-
8 ment of compatible power sources [1-10]. Considering the limited lifetime and pollution problems of
9 traditional batteries that require repetitive charging, triboelectric nanogenerator (TENG) that converts the
10 distributed mechanical energy into electricity based on triboelectrification and electrostatic induction,
11 shows superiorities in wearable applications such as portable power source [11-17], self-powered sensors
12 and e-skin [18-23]. Important progress of textile-based TENGs has been achieved for unobtrusive biome-
13chanical energy harvesting [24-25], as well as continuous, real time, and noninvasive health monitoring
14 [26-29]. Mechanical compliance and stretchability of TENGs exhibit increasing importance for seamlessly
15 integrated wearable applications. Elastic polymers such as polydimethylsiloxane (PDMS) [30-31], silicone
16 rubber [32], ethylene-vinyl acetate (EVA) [33] have been widely utilized for fabrication of stretchable
17 TENG. However, these elastic rubbers are airtight and may cause skin discomfort or even induce inflam-
18 mation for long-term wearable electronics [34].

19 In comparison, electrospun membranes with superior breathability, great flexibility, controllable
20 thickness and ease of manufacturability, show great potential for wearable devices [35-39]. Furthermore,
21 electrospinning is capable of producing membranes with micro/nano architectures and high surface rough-

1 ness, which could effectively improve the contact area and friction effect to enhance the output perfor-
2 mance of triboelectric materials [40-42]. A wide range of electrospun nanofibers has been successfully
3 applied to fabricate wearable devices. For example, Li et al. presented an all-fiber based e-skin fabricated
4 with polyvinylidene fluoride (PVDF) nanofibers, carbon nanofibers and polyurethane (PU) nanofibers,
5 while both the triboelectric and electrode layers are non-stretchable [34]. Liang et al reported a stretchable
6 TENG based on polytetrafluoroethylene (PTFE)-PU bilayer membrane and PU-Ag nanowire electrode.
7 However, VHB tapes and a hot-press process are needed for device assembly and the stretchability of the
8 device relies on PU [43]. Some other stretchable electrospun membranes such as PU/carbon nanotubes
9 (CNT)-cellulose nanocrystals (CNC) composites [44], PU-Ag nanowire network [45-46] were also
10 demonstrated as strain sensor or epidermal electrode, in which their deformability also relies on PU. It is
11 challenging to maintain high stretchability as well as strong adhesion between PU and other functional
12 layers, which could affect the deformability and durability of the device. So far, electrospun nanofiber
13 membranes are limited in deformability, in particular the stretchability has been less than satisfactory due
14 to the irreversible sliding of the physically stacked nanofibers, which highly restrains the seamless integra-
15 tion with daily textiles and human body for wearable applications. Although some methods have been
16 attempted to improve the deformability and elasticity of nanofibers materials, such as addition with elas-
17 tomer [47], decorating with extra coating [48], and thermal crosslinking [49], they suffer from tedious
18 fabrication, reduced air-permeability and high temperature requirement. At present, limited efforts have
19 been channeled onto a one-step strategy at room temperature on the development of nanofiber membranes
20 with intrinsic stretchability in commensurate with highly stretchable electrodes and deformable textiles,
21 which is critical in realizing TENGs with good mechanical compliance for wearable e-textile.

1 Herein, electrospinning of poly (vinylidene fluoride-co-hexafluoropropylene) (PVDF-HFP) assisted
2 with simultaneous electrospraying of styrene-ethylene-butylene-styrene (SEBS) was performed to fabricate
3 the first breathable nanofibers-membrane with high stretchability and hydrophobicity. The co-deposited
4 SEBS elastomer serves as microsphere-binders among the PVDF-HFP nanofibers, capable of anchoring
5 the nanofibers at distributed location to facilitate reversible fibers sliding upon stretching and therefore
6 enhancing the stretchability. SEBS microspheres also increase hydrophobicity of the PVDF-HFP nano-
7 fibers-membrane due to the improvement of surface roughness. The obtained PVDF-HFP/SEBS (PHS)
8 membrane has controllable thickness (from nanometers to microns), high stretchability (ultimate strain of
9 ~490%), great hydrophobicity (static water contact angle (WCA) of ~140°) and breathability (71% of cot-
10 ton). The stretchable nanofibers-based TENG (SNF-TENG) with effective area of $2 \times 2 \text{ cm}^2$ shows
11 output voltage of 85 V and instantaneous power density of 219.66 mW m^{-2} , which is able to power 200
12 light-emitting diodes (LEDs) array and an electronic watch. The PHS membrane exhibits excellent inte-
13 grability with stretchable textile, demonstrating multifunctional applications such as self-powered touch or
14 posture sensors, smart raincoat as well as tactile interactive interfaces. The electrospinning-electrospraying
15 integrated technique provides an effective route for fabrication of highly stretchable nanofiber membranes,
16 delivering an attractive feasibility for applying the nanofibers membranes to wearable electronic devices
17 and human-robot interactions.

18 **2 Results and discussion**

19 *2.1 Fabrication of self-interlocked stretchable nanofibers based TENG*

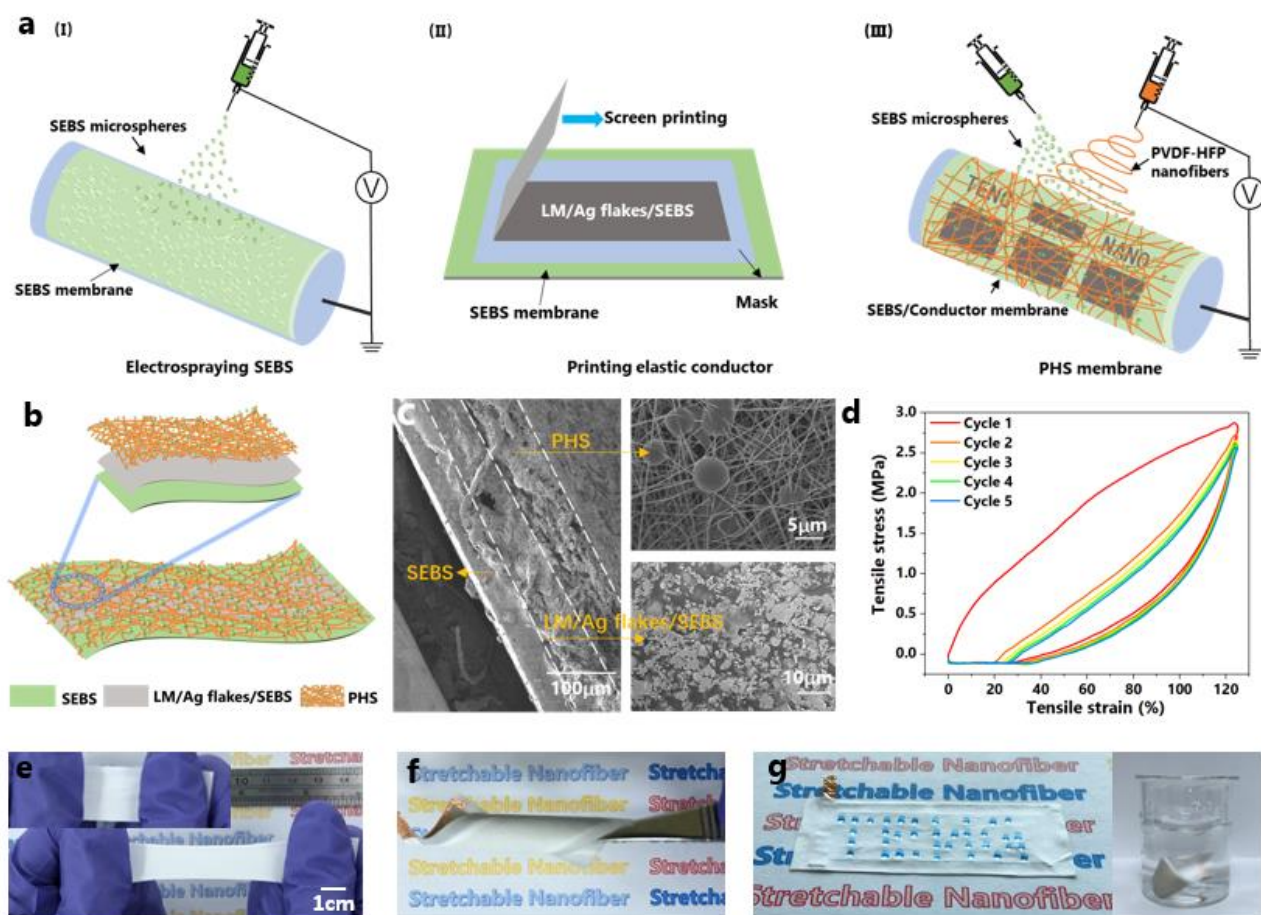
20 Block copolymers are known to self-assemble into ordered phase with various periodic nanostructures
21 through electrospinning by selecting suitable solvents, copolymer molecular weight or relative volume frac-

1 tion between the blocks [50-52]. SEBS is a triblock copolymer of polystyrene (PS) and poly (ethylene bu-
2 tylene) (PEB) with great elasticity, electrospinnability and biocompatibility [52]. PVDF-HFP shows strong
3 electronegativity, hydrophobicity and high chemical stability, which has been widely used as triboelectric
4 layer for TENGs [53-54]. Moreover, electrode with advanced deformability and conductivity is significant to
5 stretchable TENGs considering that robust adhesion among the substrate, electrode and triboelectric layer
6 determines the mechanical durability of the device [55]. Herein, we designed SEBS microspheres by elec-
7 trospaying with cosolvent system to alter the selective solubility of disparate polymer blocks, forming a
8 self-assembled stretchable SEBS dense membrane with considerable surface roughness (Fig. 1a(I)). A sus-
9 pension of liquid metal (gallium indium tin (GaInSn), LM) and silver (Ag) flakes in SEBS resin was
10 prepared and deposited onto the SEBS membrane by screen printing (Fig. 1a(II)) to prepare the stretchable
11 conductor. The strategy shows merits of stretchability, conductivity and seamless integratability with the
12 substrate. The resultant conductive SEBS membrane was used as the collector during PVDF-HFP electro-
13 spinning as shown in Fig. 1a(III). The electrospaying was performed simultaneously to deposit SEBS elastic
14 microspheres as binders to interlock the electrospun PVDF-HFP nanofibers, generating a PHS membrane
15 with high stretchability, breathability and waterproofness on the electrode.

16 A sandwiched SNF-TENG was assembled as shown in Fig. 1b, three layers are tightly adhered to each
17 other due to the in-situ interlocking deposition technique (Fig. 1c), ensuring a 175 μm thick SNF-TENG with
18 good deformability and durability. PHS nanofibers-membrane serves as the triboelectric layer. SEM image at
19 top right of Fig. 1c reveals that PVDF-HFP nanofibers were well locked by the SEBS microspheres, provid-
20 ing stable hierarchical/interlocked architectures with distinct rough surface. Importantly, such an interlocked
21 structure exerted on the PVDF-HFP nanofibers could effectively adjust the tensile stress distribution with the

1 help of soft elastomeric SEBS that buffers the stress by absorbing more energy at strain state, endowing the
2 PHS membrane with high stretchability and deformability. The elastic conductor also exhibited a significant
3 role that enables the seamless integration between different functional layers of SNF-TENG. The perfect fu-
4 sion of the elastic conductor and substrate layer can be achieved thanks to the utilization of the same polymer
5 matrix-SEBS. The printable elastic conductor ink with toluene as solvent will slightly dissolve the SEBS
6 substrate during the screen-printing process, resulting in an embedded interface with tight adhesion between
7 them. As the mixed solvent of 85% mesitylene/15% N,N-Dimethylformamide (DMF) for electrospaying has
8 high boiling temperature (about 160°C) that could not dried quickly, the subsequently electrospayed SEBS
9 microspheres landed on the conductive SEBS film (Fig.1a (III)) will inevitably carry little residual solvent
10 that could slightly etch the SEBS matrix in conductor. Meanwhile, the SEBS microspheres serve as binder to
11 interlock the PVDF-HFP nanofibers network, enabling the tight mechanically merging between the triboe-
12 lectric layer and electrode. Therefore, commendable integration between substrate, electrode and PHS layers
13 can be achieved thanks to the utilization of SEBS binder, which guarantees the mechanical stability of the
14 SNF-TENG even at strain of ~125% (Fig. S1). The device shows great recovery upon tensile load-
15 ing-unloading cyclic test (125% strain), indicating high energy dissipation enabled by the stretchable PHS
16 membrane (Fig. 1d). Slight residual strain (~21%) was observed for the first unloading cycle, owing to the
17 inherent thermoplasticity of PVDF-HPF in which energy was dissipated for the polymer chains disentangle-
18 ment. Ultimately, the SNF-TENG possesses great flexibility, stretchability, hydrophobicity and washability
19 (Fig. 1e-g), bringing promises for wearable applications.

20



1
 2 **Fig. 1.** Structure and properties of self-interlocked stretchable nanofiber based TENG (SNF-TENG). (a)
 3 Schematic illustration of the fabrication process of the SNF-TENG. (i) Electro spraying to assemble SEBS
 4 membrane, (ii) Screen printing of stretchable electrode on SEBS membrane, (iii) Simultaneous deposition of
 5 PVDF nanofibers and SEBS microspheres on the conductive SEBS membrane. Electrode pattern shows the
 6 feasibility of this in-situ deposition and assembly technology to fabricate SNF-TENGs with desirable ge-
 7 ometrics. (b) Structure of the designed SNF-TENG with sandwich-like architecture. (c) Cross-sectional SEM
 8 image and surface morphology of the SNF-TENG. (d) Cyclic tensile properties of PHS based SNF-TENG.
 9 (e-g) Photographs demonstrating the stretchability, flexibility, hydrophobicity and washability of
 10 SNF-TENG.

11 The same method is also adopted for textile-TENG fabrication by replacing the SEBS substrate to knit-
 12 ted polyethylene terephthalate (PET) or other highly stretchable textiles, indicating the advantages of this
 13 integrated technology by screen printing of elastic conductor and in-situ deposition of stretchable nanofibers

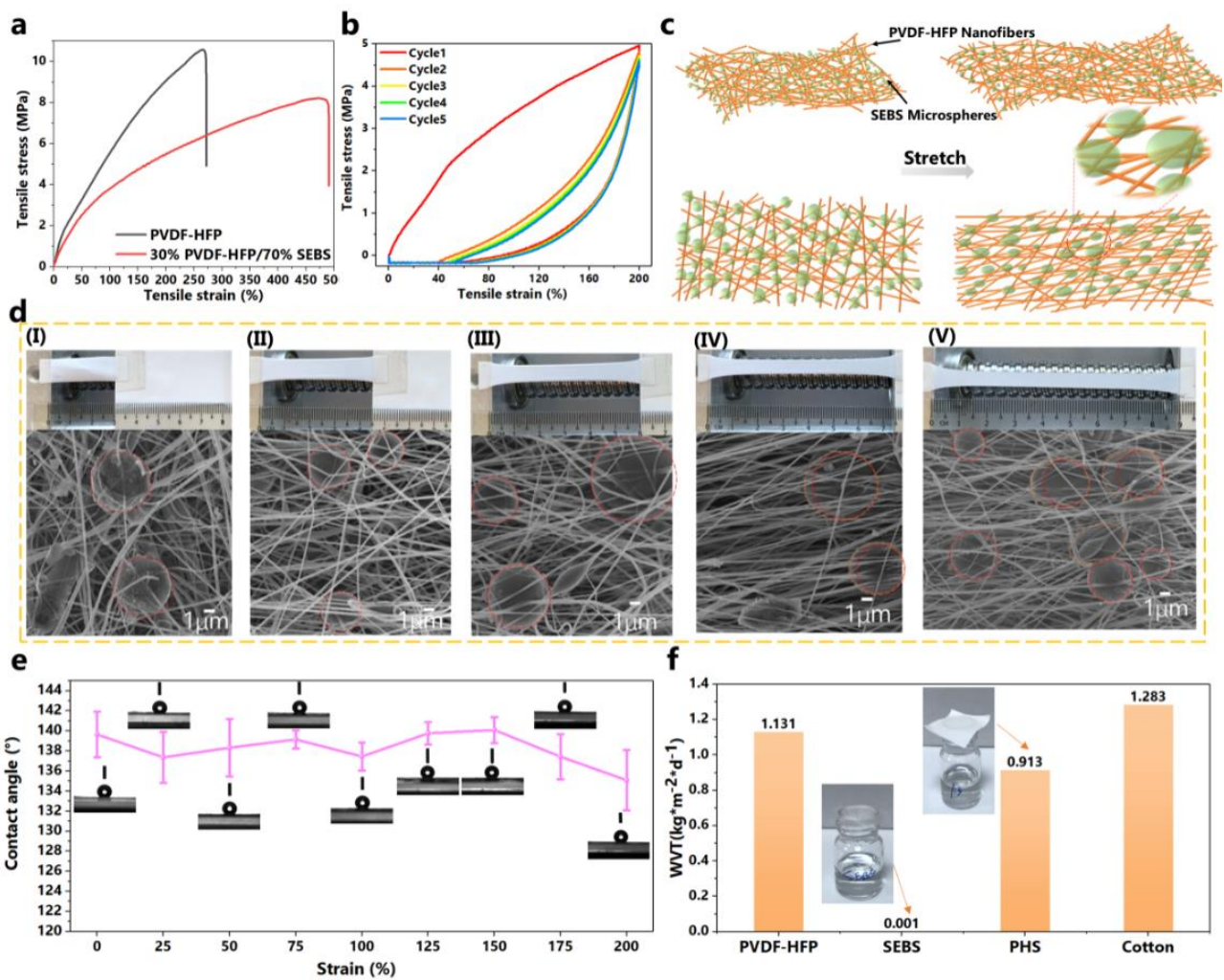
1 triboelectric layers that could achieve seamless integration of functional stretchable nanofibers and fabrics.

2 *2.2 Stretchability, hydrophobicity, and breathability of PHS membrane*

3 As the properties of PHS membrane highly rely on the content of PVDF-HFP and SEBS, a series of
4 PHS membranes with different weight ratios of PVDF-HFP/SEBS were fabricated by controlling the feeding
5 rate of polymer solutions through simultaneously electrospinning and electrospraying (Fig. S2). SEM images
6 in Fig. S3 show the composite membranes comprising of PVDF-HFP nanofibers embedded with different
7 amount of SEBS microspheres. FTIR reveals that there is no additional chemical bonding formation between
8 the two components, therefore it is conjectured that the PHS membranes were physically interlocked rather
9 than chemical interaction (Fig. S4).

10 Normally, PVDF-HFP nanofiber membranes are prone to delamination upon contacting with other ma-
11 terials due to the weak adhesion between the stacked nanofiber layers, resulting in poor mechanical stability
12 [34]. In comparison, the PHS membrane with the same thickness as the PVDF-HFP nanofiber membrane
13 exhibited no delamination between nanofibers after continuous vertical contact-separation with aluminum
14 film or air flow blown (Fig. S5). Its robust structure stability is due to the interlayer locking between
15 PVDF-HFP nanofibers and SEBS microspheres, which was verified by the cross-section SEM observation
16 shown in Fig. S6. The effect of the amount of SEBS microspheres on the tensile properties of PHS mem-
17 branes are given in Fig. S7. The elongation at break of the PHS membranes was enhanced with increasing
18 SEBS content. PHS membrane with the weight ratio (PVDF-HFP: SEBS) 1:9, 3:7, 5:5 can sustain tensile
19 strains of 1400%, 490% and 304% respectively, which are higher than that of pure PVDF-HFP nanofibers
20 membrane (~270%). In addition, the Young' modulus values decrease with the increase of SEBS content in
21 the PHS membranes (Tab. S1). All the PHS membranes demonstrate lower Young' modulus than that of

1 PVDF-HFP. This confirms that the addition of SEBS microspheres delivers better softness to the PHS mem-
 2 brane, which will effectively dissipate the energy upon deformation. A higher tensile strain for
 3 30%PVDF-HFP/ 70%SEBS membrane (~490%) than that of PVDF-HFP nanofibers membrane (270%) can
 4 be shown in Fig. 2a. Thus, it is evident that the interlocked networks of PVDF-HFP nanofiber by SEBS mi-
 5 crospheres could effectively enhance the stability, stretchability and deformability of PHS membrane.



6
 7 **Fig. 2.** Properties of the PHS membrane. (a) Tensile stress-strain curves of the pure PVDF-HFP and PHS
 8 (30% PVDF-HFP, 70% SEBS) membrane. (b) Cyclic tensile stress-strain curve of PHS membrane (30%
 9 PVDF-HFP, 70% SEBS). (c) Schematic of the stretchable mechanism of PHS membrane. The orange line
 10 represents PVDF-HFP nanofiber and the light green circle or ellipse represents SEBS microspheres. (d)
 11 Photograph and SEM images of the PHS membrane (30% PVDF-HFP, 70% SEBS) at (I) 0%, (II) 50%, (III)

1 100%, (IV) 150% and (V) 200% strain. (e) Static water contact angle (WCA) of PHS membrane (30%
2 PVDF-HFP, 70% SEBS) at different strain. (f) Water vapor transmittance (WVT) rates of the PVDF-HFP,
3 SEBS, PHS membrane (30% PVDF-HFP, 70% SEBS) and cotton.

4 Meanwhile, the desired balance between tensile properties and triboelectric performance is a key pa-
5 rameter for SNF-TENG. According to Fig. S8, output voltage of devices based on the PHS membranes with
6 higher PVDF-HFP content exhibit higher values at the same condition. The PHS membranes with the
7 PVDF-HFP/SEBS weight ratio of 1:9, 3:7, 5:5 show output voltage of 33 V, 93 V and 131 V respectively,
8 which is 24%, 70% and 97% that of pure PVDF-HFP (135 V). The reducing voltage output of the PHS
9 membranes with higher SEBS weight ratio could be ascribed to the lower triboelectric affinity of SEBS
10 compared to PVDF-HFP. Having too much SEBS microspheres (>90%) with tiny PVDF-HFP nanofibers
11 could not attain a hierarchical structure with higher roughness as most of the PVDF-HFP nanofibers were
12 covered by the aggregation of SEBS (as shown in Fig. S3). Considering both stretchability and triboelectric
13 performances, we selected 3:7 (PVDF-HFP: SEBS) as the optimal weight ratio for PHS membrane fabrica-
14 tion. Further mechanical performance tests were conducted (as shown in Fig. S9). The PHS membrane (30%
15 PVDF-HFP/70% SEBS) shows increased residual strain (7.5% ~ 40%) mainly at the first loading-unloading
16 cycle when the tensile strains increased from 50%, 100%, 150% to 200%. It suggests that partial physical
17 displacement occurred between nanofibers, together with loss of strain energy in the form of irrecoverable
18 heat energy as generated by the sliding of PVDF-HFP thermoplastic molecule chains over each other [56-57].
19 Thereafter, lower tensile stresses were attained and PHS membrane showed favorable recovery even by ap-
20 plying 200% tensile strain for 5 cycles (Fig. 2b). It indicates the movement of polymeric molecule chains
21 reached a relative stable condition due to the constraint of elastomeric SEBS microspheres. Tensile strain of
22 100% was applied on the PHS membrane at different strain rates (50-150 mm min⁻¹), which verified that no

1 obvious impact on the recoverability of material (Fig. S10). From the digital photos taken, there are no visi-
2 ble damages observed on the PHS membrane at strain of ~200% (Fig. S11). It indicates that PVDF-HFP
3 nanofibers membrane could recover well upon cyclic stretching, performing as an elastic membrane.

4 The stretchability mechanism of PHS membrane can be schematically explained (as shown in Fig. 2c).
5 The PHS membrane consists of SEBS microspheres randomly embedded within the curly PVDF-HFP nano-
6 fibers (Fig. 2d (I)). Once the membrane is stretched (~50%), the random PVDF-HFP nanofibers are tightened
7 along the stretching direction firstly (Fig. 2d(II)), sustaining most of the tension distributed within and on the
8 surface of the PHS. The realignment is almost an irrecoverable process, generally leading to residual strain.
9 As the strain increases to 100%, PVDF-HFP nanofibers are further tightened (Fig. 2d (III)) and the dis-
10 placement begins to be increasingly restrained by the embedded SEBS microspheres. When further
11 increasing the strain to 150% and 200%, apparent deformation was observed on the SEBS microspheres,
12 which was induced by the increasing displacement between nanofibers that have been fully tightened (Fig.
13 2d (IV)) and partial fibers were being damaged due to the over loading (Fig. 2d (V)). In addition, the exist-
14 ence of SEBS microspheres with circular shapes at 200% strain is due to the stress mostly concentrated on
15 the PVDF-HFP nanofibers, suggesting that only partial SEBS microspheres are subjected to the tensile stress
16 at 200% strain. Therefore, higher breaking elongation of ~490% can be achieved (Fig. 2a). During the
17 stretching processes, SEBS microspheres play an important role as the binder to effectively limit the physical
18 sliding of PVDF-HFP nanofibers. The elastic network constructed by SEBS microspheres is capable of dis-
19 sipating the tensile stress to well recover the stretched nanofibers membrane in shape. Therefore, the PHS
20 membrane with structure of co-deposited nanofibers and elastic microspheres shows superior stretchability
21 than that of the commonly fabricated electrospun nanofibers [35-37].

1 The hierarchical network of nanofibers and microspheres also bring superior waterproofness to the PHS
2 membrane. As shown in Fig. S12, electrospayed SEBS and electrospun PVDF-HFP membranes are both
3 intrinsic water-resistant materials with the static WCA of 103° and 132° . PHS membranes with PVDF-HFP
4 weight content higher than 20% all have an apparent WCA of around 140° , which could be mainly ascribed
5 to the SEBS microspheres that roughened the surface (Fig. S3), enabling trapped air in the pores with out-
6 ward pressure to resist the penetration of water droplet [58]. The surface wettability is determined
7 cooperatively by its morphology (surface roughness) and intrinsic material properties (surface energy) [59].
8 The hydrophobic surface can be obtained by directly electrospinning a hydrophobic polymer or modifying
9 the rough surface with a low-surface-energy material [60]. Herein, the PHS membranes with 50-80% content
10 of SEBS microspheres show comparable WCAs around 140° (Fig. S12), indicating 50% content of SEBS
11 microspheres embedded into the PVDF-HFP nanofibers is enough to construct a favorable micro-nano hier-
12 archical structure with enhanced hydrophobicity. Further increasing the SEBS content could not improve the
13 WCA, but endowing PHS membrane with higher stretchability. The self-interlocked hierarchical architec-
14 tures ensure the stable hydrophobicity of the PHS membrane even upon stretching up to $\sim 150\%$. Slight
15 decreased WCA was observed on a typical PHS membrane (30% PVDF-HFP/ 70%SEBS) with tensile strain
16 higher than 150% (Fig. 2e), which is due to the increased capillary effect of aligned nanofibers upon higher
17 stretching. The stable WCA suggests there is no large change in the surface roughness of the PHS membrane
18 upon stretching, which is of significance to maintain the triboelectric properties under extreme stretching
19 conditions.

20 Additionally, considerable air permeability is attainable owing to the favorable porosity of PHS mem-
21 branes. Normally, the air permeability could be evaluated by the Fickian diffusion of water vapor through the

1 porous structure, which is driven by the relative humidity between two sides [34, 61]. Thus, water vapor
2 transmittance (WVT) rate was applied here to explore the breathability of PHS membranes. The samples
3 were covered on bottles contained water to monitor the weight change of the setup, normalizing as WVT. Fig.
4 2f shows that the WVT of the 3:7 PHS membrane reaches 80% of PVDF-HFP, 71% of cotton and no water
5 droplets accumulation can be found at its inner surface (Fig. S13). Overall, the in-situ deposited SEBS mi-
6 crospheres act as elastomeric binders and hydrophobic modifiers for enhancing the deformability and
7 waterproofness of PVDF-HFP, endowing the higher stretchability, hydrophobicity, breathability and triboe-
8 lectric performance to the composite membrane. These compelling features render the self-interlocked
9 stretchable PHS membrane highly desirable for wearable triboelectric devices.

10 *2.3 Energy harvesting performance of SNF-TENG*

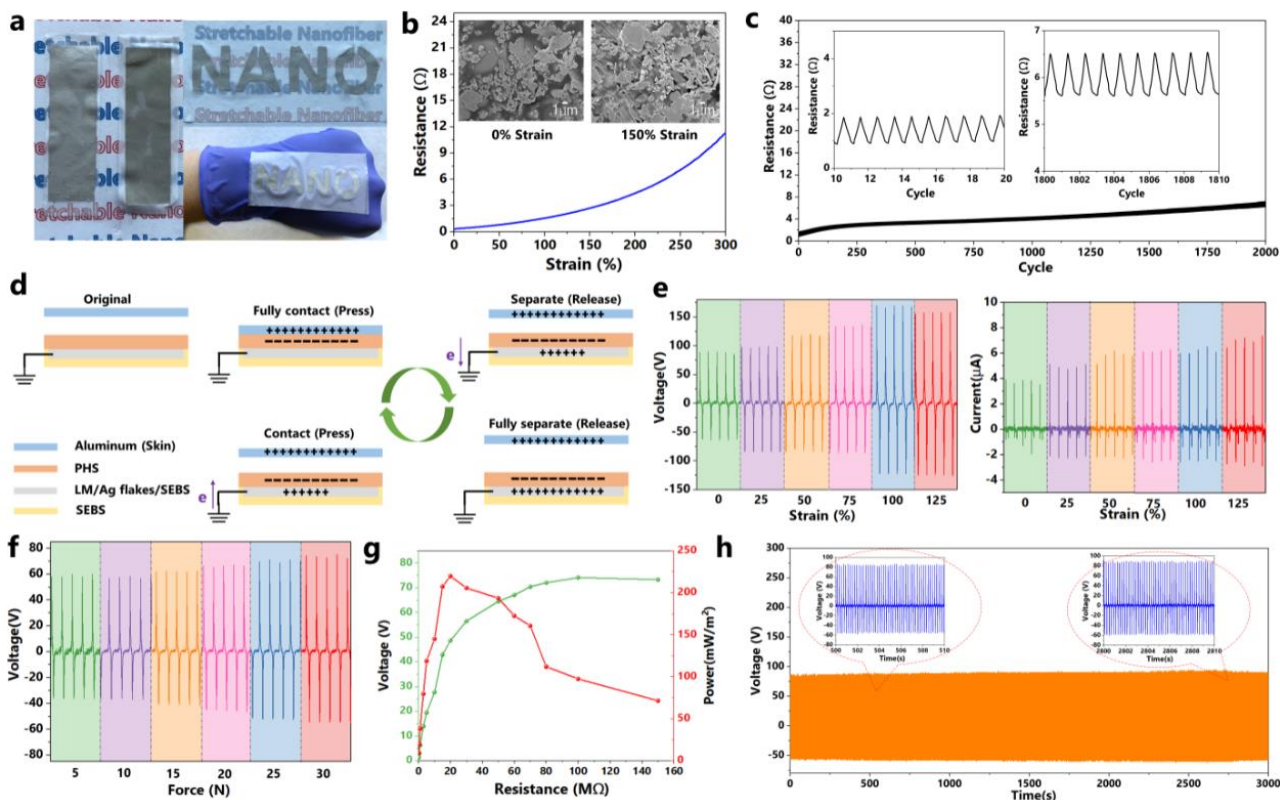
11 Admittedly, flexible and stretchable electrode is an essential component for TENGs and the mechanical
12 durability among different functional layers needs to be addressed. Printable elastic conductor consists of
13 conductive fillers and polymer matrices with great conductivity, stretchability, substrate adaptability and
14 durability, is promising for wearable devices [62]. Here, we synthesized LM-Ag flakes-SEBS elastic con-
15 ductor (relevant details can be found in Fig. S14 and experimental section) using as stretchable electrode for
16 SNF-TENG. The elastic conductor is capable of being screen printed on the SEBS substrate with different
17 geometric forms, such as rectangle or the “NANO” letter (Fig. 3a). Tight adhesion among substrate, elec-
18 trode and PHS membrane was successfully achieved (verified by the cross-sectional SEM image given in Fig.
19 1c) thanks to the matched Young’s modulus of different layers with the utilization of SEBS binder by in-situ
20 deposition technology. The elastic conductor printed on the SEBS substrate clearly displayed excellent
21 conductivity and a low resistance about 3Ω can be maintained even at 200% strain (Fig. 3b), which is as-

1 cribed to the GaInSn that can be released to reestablish the electrical interconnects between the Ag flakes as
2 shown in Fig. S15. Here, the GaInSn LM particles provide dynamic and robust electrical anchors between
3 the conductive fillers. Mechanical robustness of the electrode was also investigated by monitoring the re-
4 sistance during fatigue cycles at 150% strain. Although the resistance slightly increases, its value is still
5 lower than 7Ω after 2000 cyclic tests (Fig. 3c). The change is negligible for output performance owing to the
6 large impedance of TENGs [63].

7 The mechanical energy harvesting mechanism of the SNF-TENG can be explained as shown in Fig. 3d.
8 The electricity generation originates from contact electrification and electrostatic induction [64-65]. Firstly,
9 when the alien surface (aluminum or skin) contacts with the PHS membrane, electrification occurs owing to
10 the charge transfer between them. The net negative static charges are generated on the PHS membrane due to
11 its higher surface electron affinity. Once the two surfaces are separated to a certain distance, an electrical
12 potential difference (voltage) is built and the negative charge on the PHS membrane induces positive charge
13 to the electrode. Free electrons flow from the electrode to ground, generating the current pulse. The electro-
14 static equilibrium is achieved once the alien surface and PHS membrane reaches the maximum displacement.
15 As the alien surface moves to the PHS membrane again, the induced positive charges in the electrode de-
16 creases (the electrons flow back to the electrode) and a reversed output signal generates. The continuous
17 contact-separation process will generate voltage and current pulse, converting mechanical energy to electric-
18 ity.

19 The output performance of SNF-TENG ($2 \times 2 \text{ cm}^2$ area) under different tensile strain conditions was
20 investigated by applying tapping force of 30 N at 5 Hz (Fig. 3e). The output voltage (V_C), short-circuit cur-
21 rent (I_{SC}), transferred charge (Q) of the device show an increase trend with tensile strain (Fig. S16). The V_C

1 of 85 V, I_{SC} of 4 μ A, Q of 15 nC can be detected at 0% strain and their value reaches 160 V, 7 μ A, 29 nC at
2 100% strain. The increase of output performance is attributed to the variations of contact area at strain state.
3 The output performance of SNF-TENG under different applied forces, contact frequencies were also inves-
4 tigated. The device shows a V_C of \sim 60 V at 5 N, indicating it could be easily triggered (Fig. 3f and Fig. S17).
5 The V_C , I_{SC} and Q show a mild increase trend with contact frequency lower than 8 Hz, and commence a re-
6 duction when the contact frequency is higher than 10 Hz (Fig. S18). The lower output voltage at 2 Hz and 14
7 Hz were attributed to the insufficient charge transfer due to long separation or transient contact. The power
8 output performance of SNF-TENG was evaluated by varying different external load resistors. As shown in
9 Fig. 3g and Fig. S19, the output voltage of SNF-TENG gradually increases from 2.88 V to 73.28 V as the
10 external load changes from 500 k Ω to 150 M Ω . The output current shows decreasing trend with the increase
11 of load resistance. The extracted maximum instantaneous peak power density of 219.66 mW m⁻² is achieved
12 at a matched resistance of 20 M Ω . Moreover, the durability test for the SNF-TENG was conducted by con-
13 tinuous contact-separation at the frequency of 5 Hz. It can be seen from Fig. 3h that there is no visible
14 change of the output voltage after long period of continuous operation for 3000 s (15000 cycles). These
15 properties present the promising potential of SNF-TENG for practical applications.



1

2 **Fig. 3.** Elastic conductor properties and triboelectric performance of SNF-TENG. (a) Demonstration of the
 3 flexibility of the elastic conductor. (b) Resistance-tensile strain curve of the elastic conductor printed on the
 4 SEBS substrate. (c) Demonstration of stable resistance of the elastic conductor under 2000 cycles of 150%
 5 tensile strain. (d) Working mechanism of the SNF-TENG. (e) Output performance of the SNF-TENG under
 6 different tensile strain state. (f) Output performance of the SNF-TENG under different applied force. (g)
 7 Dependence of voltage and instantaneous peak power density of the SNF-TENG under different resistance
 8 load conditions ($P = I^2R$). (h) Output durability of the SNF-TENG under continuous measurement.

9

10 The inherent waterproof properties of SEBS and PHS membranes render the promising application of
 11 SNF-TENG in water environment. Here we demonstrated the SNF-TENG that is capable of harvesting water
 12 energy with high output and remarkable robustness. The working mechanism of liquid-solid triboelectrifica-
 13 tion shown in Fig. 4a is similar to that of mechanical energy harvesting, which relies on the contact
 14 electrification and electrostatic induction process between water droplets and PHS membrane. The hydro-
 phobic surface allows water droplets to slide away quickly and avoid the formation of residual liquid film,

1 which enables complete charge transfer in each cycle and ensures the high output performance of the device.

2 The output performance of a SNF-TENG with area of $3 \times 3 \text{ cm}^2$ was investigated under flowing water.

3 The output voltage and current increase with the water speed in the range of $4.03\text{-}11.33 \text{ ml s}^{-1}$ and then de-

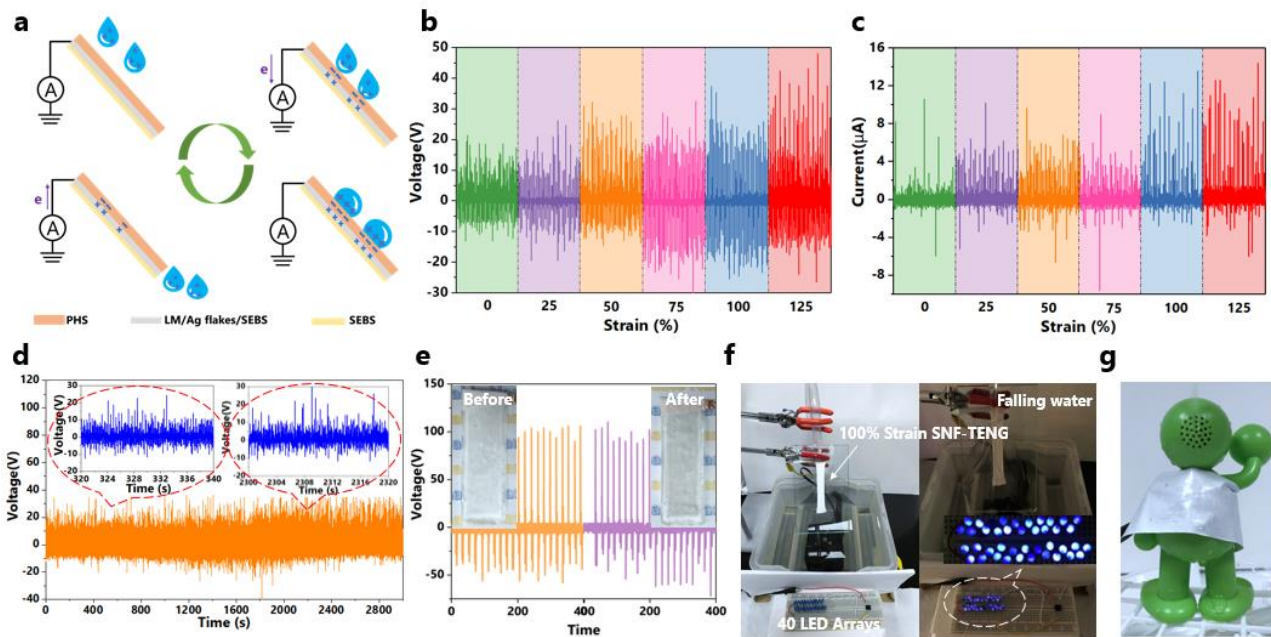
4 creases (Fig. S20). The highest V_C , I_{SC} reaches 65 V and $16 \mu\text{A}$ at the speed of 11.33 ml s^{-1} . In addition, we

5 found that the optimal device-vertical angle (defined as the angle between device and the vertical direction)

6 is around $30^\circ\text{-}45^\circ$ (as shown in Fig. S21-22). The lower device-vertical angle results in insufficient contact

7 between water droplets and PHS membrane, while higher value will generate residual liquid film on the de-

8 vice surface, screening the charge generation and suppressing the complete electron transfer in each cycle.



9

10 **Fig. 4.** Performance of the SNF-TENG under water driven mode. (a) Water energy harvesting mechanism of

11 the SNF-TENG. (b-c) Output performance of the SNF-TENG for water energy harvesting under tensile

12 strain conditions. (d) Output durability of the SNF-TENG. (e) Output performance of the SNF-TENG before

13 and after extended washing of 15 h. (f) Demonstration of the SNF-TENG that drives 40 LED arrays under

14 water flow at 100% strain. (g) Demonstration of the smart raincoat for electricity generation.

15 The performance of the water driven SNF-TENG under different tensile strain states was also investi-

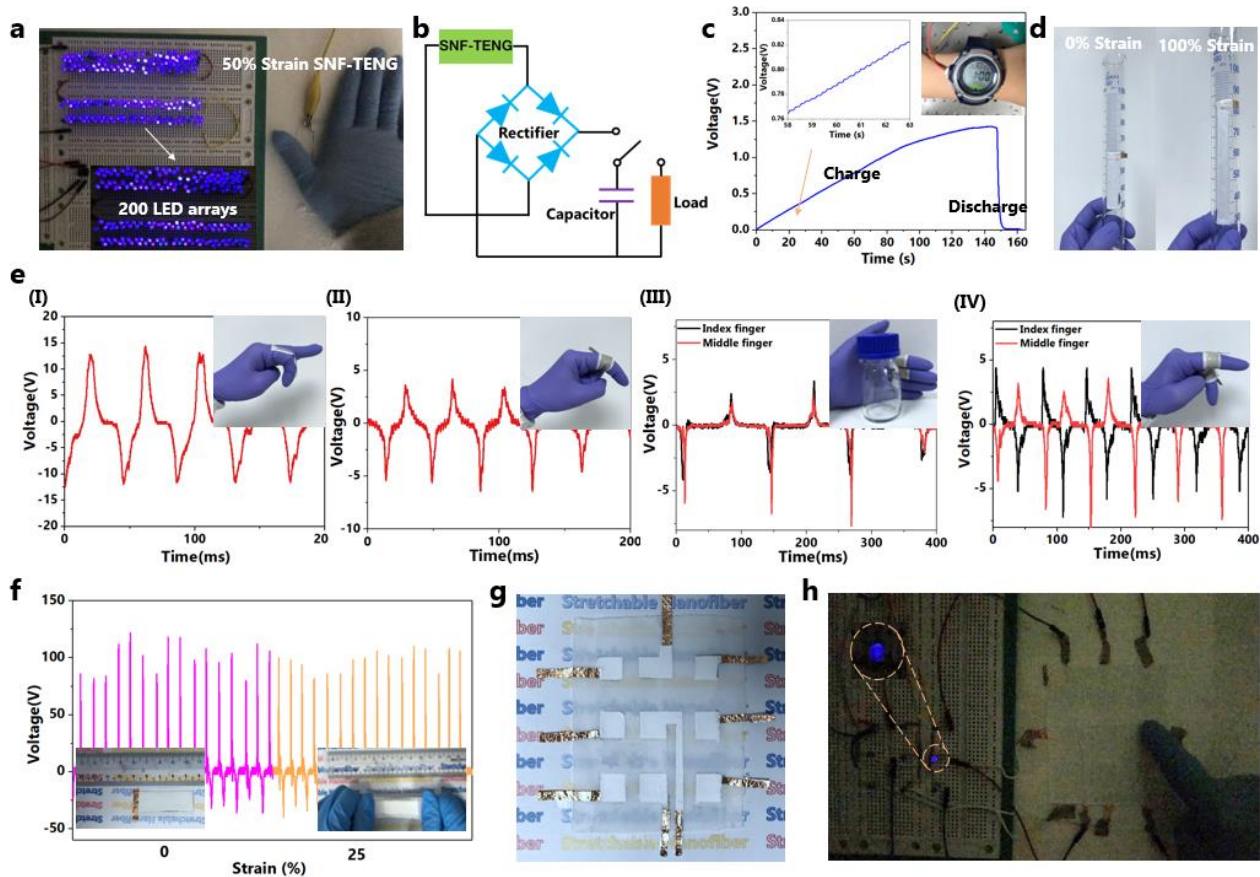
1 gated, as shown in Fig. 4b-c. The output voltage achieves approximately 45 V at 125% strain (higher than
2 that of 20 V at 0% strain), which is mainly ascribed to the effective area increase of the device at strain state.
3 The great durability of SNF-TENG delivers a water energy harvester with reliable output for continuous
4 working (Fig. 4d). The output voltage of the SNF-TENG that underwent 15 h washing still remains stable,
5 suggesting an admirable robustness of the device (Fig. 4e). Moreover, the SNF-TENG ($1.5 \times 4.5 \text{ cm}^2$ area,
6 Fig. S23) could easily power 40 LED arrays without batteries by water flow at 100% tensile strain state (Fig.
7 4f, Supplementary Video S1). The SNF-TENG is also capable of working as wearable raincoat based on a
8 device with the letter “TENG” patterned electrode (Fig. S24), which shows a stable output voltage of 24 V
9 under 8.4 ml s^{-1} flowing water (Fig. 4g). Benefiting from the customizable electrode and self-assemble PHS
10 membrane, it is easy to employ other complex substrates to fabricate wearable smart raincoats.

11 *2.4 SNF-TENG for power sources and self-powered sensing*

12 The self-interlocked stretchable PHS based SNF-TENG demonstrates multiple application potentials.
13 Firstly, the SNF-TENG can scavenge mechanical energy of human motions. As demonstrated in Fig. 5a and
14 Supplementary Video S2, 200 LED arrays could be easily lighted up when tapping a SNF-TENG (4.5×4.5
15 cm^2 area) with hand both at 0% and 50% strain (Fig. S25). The generated electricity can be collected and
16 stored to power different portable electronics based on the equivalent circuit shown in Fig. 5b, wherein the
17 rectifier bridge and capacitor are utilized to alternate the SNF-TENG outputs and store the electricity, re-
18 spectively. Various capacitors (22-100 μF) can be charged by the SNF-TENG ($4.5 \times 4.5 \text{ cm}^2$ area) to meet
19 different application requirements (Fig. S26). Fig. 5c depicts the real-time charging curve of a 33 μF capaci-
20 tor driven by the SNF-TENG. The capacitor voltage reached 1.43 V within 140 s by hand tapping the device
21 and the voltage-step curve for the charging process is apparent (inset of Fig. 5c). The stored electricity in the

1 capacitor is able to power a wearable electronic watch without battery, the discharging curve of the capac-
2 itor was also given. The SNF-TENG could be attached to a variety of objects surface and serve as power
3 source thanks to its flexibility, stretchability and shape adaptability (Fig. 5d).

4 Given the great mechanical adaptability of PHS membrane, the SNF-TENG can be utilized as
5 self-powered e-skin. As an exemplification, the SNF-TENG ($1.5 \times 4.5 \text{ cm}^2$ area) was attached on a finger
6 or worn on a finger joint and the characteristic output signals were detected by cyclic finger bending. When
7 the e-skin is attached on the finger, the positive and negative output signal shows similar value ($\sim 12.5 \text{ V}$),
8 which may attribute to the comparable contact-separation amplitude between the e-skin and finger (Fig. 5e I,
9 Supplementary Video S3). However, the e-skin that worn on a finger joint works in the bending mode gener-
10 ates different waveform signals (Fig. 5e II, Supplementary Video S3). The amplitude of the negative output
11 voltage value ($\sim 6 \text{ V}$) is higher than the positive one ($\sim 3 \text{ V}$), owing to the deformation degree of the e-skin
12 during the bending process is higher than the straighten process. Furthermore, the e-skin could be worn on
13 multiple fingers to reveal complex motions. The synchronous in-phase signal of the e-skins worn on the in-
14 dex finger and middle finger joints can be detected when grabbing and releasing a bottle by hand (Fig. 5e III
15 and Supplementary Video S4). And the synchronous out-of-phase signal could also be measured when the
16 index finger and middle finger bend alternately (Fig. 5e IV and Supplementary Video S4). Thereupon, this
17 e-skin shows a promising smart application such as self-powered feedback sensors in robots, remote control-
18 lers as well as continuous healthcare monitoring in real-time.



1

2 **Fig. 5.** SNF-TENG and textile-TENG work as power sources or sensors. (a) SNF-TENG drives (4.5×4.5
 3 cm^2) 200 LED arrays by tapping. (b) Circuit diagram for SNF-TENG works as power source for electronic
 4 device. (c) SNF-TENG as power sources to charge a $33 \mu\text{F}$ capacitor for powering an electronic watch. (d)
 5 Stretchability demonstration of the SNF-TENG. (e) The characteristic output signal of the SNF-TENG ($1.5 \times$
 6 4.5 cm^2) under different finger motions. (f) Output performance of textile-TENG ($1.5 \times 4.5 \text{ cm}^2$) at 0% and
 7 25% strain. (g-h) Demonstration of textile-TENG based tactile interactive interface that is able to map dif-
 8 ferent touch events.

9 Considering textile is an ideal substrate with excellent deformability, breathability and compatibility for
 10 incorporation with our daily clothes [26-27]. The printable elastic conductor with great adaptability to dif-
 11 ferent substrates provides possibility for seamless integration of deformable textile and PHS membrane to
 12 fabricate a stretchable, wearable textile-TENG. Herein, the knitted PET textile based TENG with great ten-
 13 sile recovery capability after cyclic stretching was successfully assembled (as demonstrated in

1 Supplementary Video S5). The excellent interlayer adhesion among the elastic conductor, PHS membrane
2 and PET textile can be achieved owing to the in-situ self-interlocked fabrication process as well as the binder
3 enhancement of SEBS. The output performance of the textile-TENG ($1.5 \times 4.5 \text{ cm}^2$ area) driven by hand
4 tapping keeps stable (around 125 V) at 0% and 25% strain, verifying the durability of device (as shown Fig.
5 5f and Supplementary Video S6). And the textile-TENG integrated on the cloth also exhibits favorable tribo-
6 electric outputs (Fig. S27). Owing to the linear response output of the textile-TENG at different pressure, it
7 can be applied as tactile sensor with the detected sensitivity of 0.68 V kPa^{-1} in the pressure range of 8-89 kPa
8 and response time of 3.14 ms by finger tapping (as shown in Fig. S28-29). Furthermore, we fabricated a tex-
9 tile based tactile interactive interface embedded with 9 touch sensor unit ($1 \times 1 \text{ cm}^2$ area) and connected it
10 to 9 LEDs (Fig. 5g). The textile based tactile interactive interface is able to map the finger touch behavior in
11 a real time by lighting corresponding LED without any power supply (Fig. 5h and Supplementary Video S7),
12 showing a wearable interface with great potential for self-powered security or interactive entertainment sys-
13 tem.

14 **3 Conclusions**

15 In summary, we accomplish a self-interlocked stretchable, hydrophobic and breathable nanofiber mem-
16 brane derived from an innovative strategy of simultaneously electrospinning and electrospraying. The in-situ
17 deposited SEBS microspheres act as elastic binder and hydrophobic modifier, realizing a stretchable nano-
18 fibers-based membrane with favorable waterproofness and breathability. Moreover, the PHS based
19 SNF-TENG and textile-TENG demonstrated multifunctional and wearable potentials with great mechanical
20 transformability, high durability as well as exceptional energy harvesting capabilities from human motions
21 and water flow. It can drive 200 LEDs and an electronic watch easily by hand tapping as well as utilize as

1 smart raincoat, self-powered e-skin, real-time human motion sensor and tactile interactive interface in harsh
2 conditions. The development of stretchable nanofiber membrane with high hydrophobicity and breathability
3 will open new avenues for self-powered e-skin, biological behavior sensors and wearable electronic devices.

4 **4 Experimental sections**

5 *4.1 Fabrication of PHS membranes*

6 PHS membranes were fabricated by electrospinning of PVDF-HFP and electrospaying of SEBS sim-
7 ultaneously. Briefly, SEBS (S/EB weight ratio 20/80, Tuftec™ H1052) was dissolved in the Mesitylene/
8 N,N-Dimethylformamide (DMF) mixture solvent (85 %v/15 %v) by stirring (400 rpm) at 60 °C for 12 h to
9 prepare 12 wt % homogeneous solution considering that mesitylene could dissolve both PS and PEB
10 blocks, while DMF is a good solvent for the PS block only [49-50]. PVDF-HFP (Sigma-Aldrich, $M_w \sim$
11 455,000) pellets were dispersed in DMF/Acetone (60 %v/40 %v) mixture solvent by stirring (400 rpm) at
12 room temperature for 6 h to obtain 12 wt% homogeneous solution. All PHS membranes were fabricated by
13 synchronous electrospinning of PVDF-HFP and electrospaying of SEBS under the applied voltage of 20
14 kV. The weight ratio of the PVDF-HFP and SEBS was adjusted by controlling the solution feed rate (con-
15 trolled by the by syringe pump), as shown in Tab. S2. Typically, the solution feed rate for the 3:7 PHS
16 membrane is set to 0.9 ml h⁻¹ for PVDF-HFP solution and 2.1 ml h⁻¹ for SEBS solution. The distance be-
17 tween aluminum foil collector and nozzles was set to 15 cm. A heating unit with the power about 400 W
18 was used to promote solvent evaporation during the electrospinning (conducted at 70 ± 3% humidity and
19 23 ± 2°C). All the obtained membranes were dried at 60 °C for 2 h to remove the residual solvents.

1 *4.2 Fabrication of LM-Ag flakes based elastic conductor*

2 The GaInSn alloy (62% Ga, 25% In, 13% Sn, Melting point: 5 °C) and Ag flakes (Sigma-Aldrich, 10
3 μm) were used to prepare the elastic conductor. Briefly, 1.5 g GaInSn alloy was added with 6 ml toluene.
4 The GaInSn LM in toluene was sonicated for 30 min in an MRC AC-200H sonicator with the power of
5 100 W. Then the solution was stand for 30 min to precipitate liquid metal particles (as shown in Fig. S14).
6 This is followed by adding 1.5 g Ag flakes and 0.7 g SEBS resin (40 wt %), then mixing to obtain the
7 LM-Ag flakes-SEBS elastic conductor.

8 *4.3 Fabrication of the PHS based TENG*

9 Firstly, the PHS membrane based TENG was fabricated. The membrane with the $2 \times 2 \text{ cm}^2$ area
10 was fixed to a conductive double-sided tape at which the other side was pasted to the center of a commer-
11 cial PET film ($2.5 \times 6 \text{ cm}^2$ area). The other conductive double-sided tape with one side pasted to an
12 aluminum foil ($2 \times 2 \text{ cm}^2$ area) was affixed to another PET film ($2.5 \times 6 \text{ cm}^2$ area). Then the wider
13 side edges of the two PET films was pasted by a VHB tape as spacers with the thickness of 2 mm to as-
14 semble the TENG.

15 For the SNF-TENG and textile-TENG, the LM-Ag flakes elastic conductor was firstly printed on the
16 electrospayed SEBS membrane or knitted PET textile using the homemade mask. Then the printed con-
17 ductive SEBS substrate was dried at 60 °C for 15 min. Finally, the conductive SEBS membrane was
18 affixed to the collector (electrode upwards) and the synchronous electrospinning of PVDF-HFP and elec-
19 trospaying of SEBS were conducted to assemble the devices.

20 *4.4 Characterization and electrical measurement*

21 The morphology of the PHS membranes, LM-Ag flakes-SEBS conductor and the device were charac-

1 terized by a field-emission SEM (FE-SEM, JEOL 6340F). The infrared spectral characteristics of the
2 membranes were measured using Fourier Transform Infrared (FTIR) spectrometer (PerkinElmer, Frontier).
3 The static water contact angle was tested by contact angle measuring system (Dataphysics OCA15 Pro)
4 with the droplets of 5 μL . Tensile strain tests for the membranes were conducted by Static Mechanical
5 Tester (Instron, 5567). The sample was cut to the dumbbell shape following the ASTM D638 specimen
6 dimensions (Type V), as shown in Fig. S30. The resistances of the elastic conductor were measured using a
7 Keithley 2400 source meter. The customized system which consists of an amplifier (SINOCERA
8 YE5871A), a function generator (Agilent 33220A) and an electromechanical vibrator (SINOCERA
9 JZK-10) is applied to evaluate the performance of the as made TENGs. The force transducer (SINOCERA
10 CL-YD-331), oscilloscope (Tektronix MDO3024, impedance = 100 M Ω), low-noise current preamplifier
11 (SR570, impedance = 4 Ω , Stanford Research Systems) and programmable electrometer (Keithley 6514,
12 Tektronix Inc., USA) were used to measure the applied force, output voltage, short-circuit current and
13 transferred charge. The water speed was controlled by a peristaltic pump (BT100-2J). All the electrical
14 measurements were conducted in ambient environment (Temperature 23 ± 2 $^{\circ}\text{C}$; RH, $70\% \pm 3\%$). The ex-
15 periments involving human subject have been performed with the full, informed consent of the volunteer
16 and approved by the university (ref. no. IRB-2017-08-038).

17 **Acknowledgements**

18 The current work is supported by the NRF Investigatorship (NRF-NRFI2016-05) under the National
19 Research Foundation, Prime Minister's Office, Singapore. The authors (Y. Li and X. Zhang) also thank the
20 support from China Scholarship Council (Grant No. 201906270122).

21 **Author Contributions**

1 Yi Li and Jiaqing Xiong contributed equally to this work. Yi Li, Jiaqing Xiong, and Pooi See Lee
2 conceived the idea and wrote the paper. Yi Li and Jiaqing Xiong designed the scheme, fabricated the
3 membranes and devices, conducted materials characterization and analyzed the data. Jian Lv helped to
4 prepare the elastic conductor. Yi Li, Jiaqing Xiong, Jian Chen conducted the triboelectric performance tests
5 and commented on the working mechanisms. Yi Li and Dace Gao tested the tensile properties of the mem-
6 branes. Pooi See Lee and Xiaoxing Zhang supervised this project. All the authors discussed and
7 commented on the manuscript.

8 **Competing financial interests:** The authors declare no competing interests.

9 **Appendix A. Supporting Information**

10

11 **References**

- 12 [1] K. Parida, J. Xiong, X. Zhou, P.S. Lee, *Nano Energy*. 59 (2019) 237-257.
- 13 [2] K. Dong, X. Peng, Z.L. Wang, *Adv. Mater.* 32 (2020) 1902549.
- 14 [3] J. Wang, S. Li, F. Yi, Y. Zi, J. Lin, X. Wang, Y. Xu, Z.L. Wang, *Nat. Commun.* 7 (2016) 12744.
- 15 [4] M.F. Lin, J. Xiong, J. Wang, K. Parida, P.S. Lee, *Nano Energy*. 44 (2018) 248-255.
- 16 [5] L. Zhou, D. Liu, J. Wang, Z.L. Wang, *Friction*. 8 (2020) 481-506.
- 17 [6] Q. Guan, G. Lin, Y. Gong, J. Wang, W. Tan, D. Bao, Y. Liu, Z. You, X. Sun, Z. Wen, Y. Pan, *J. Mater.*
18 *Chem. A*. 7 (2019) 13948-13955.
- 19 [7] J. Wang, C. Wu, Y. Dai, Z. Zhao, A. Wang, T. Zhang, Z.L. Wang, *Nat. Commun.* 8 (2017) 88.
- 20 [8] C. Yan, Y. Gao, S. Zhao, S. Zhang, Y. Zhou, W. Deng, Z. Li, G. Jiang, L. Jin, G. Tian, T. Yang, X. Chu,
21 D. Xiong, Z. Wang, Y. Li, W. Yang, J. Chen, *Nano Energy*. 67 (2020) 104235.
- 22 [9] Z. Cong, W. Guo, Z. Guo, Y. Chen, M. Liu, T. Hou, X. Pu, W. Hu, Z. L. Wang, *ACS Nano*. 14 (2020)
23 5590-5599.
- 24 [10] D. Liu, X. Yin, H. Guo, L. Zhou, X. Li, C. Zhang, J. Wang, Z.L. Wang, *Sci. Adv.* 5 (2019). eaav6437.
- 25 [11] J. Xiong, M.F. Lin, J. Wang, S.L. Gaw, K. Parida, P.S. Lee, *Adv. Energy Mater.* 7 (2017) 1701243.

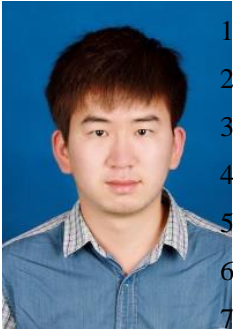
- 1 [12] X. Chen, J. Xiong, K. Parida, M. Guo, C. Wang, C. Wang, X. Li, J. Shao, P.S. Lee, *Nano Energy*. 64
2 (2019) 103904.
- 3 [13] K. Dong, X. Peng, J. An, A.C. Wang, J. Luo, B. Sun, J. Wang, Z.L. Wang, *Nat. Commun.* 11 (2020)
4 2868.
- 5 [14] Y. Chen, X. Pu, M. Liu, S. Kuang, P. Zhang, Q. Hua, Z. Cong, W. Guo, W. Hu, Z.L. Wang, *ACS Nano*.
6 13 (2019) 8936-8945.
- 7 [15] X. Liang, T. Jiang, G. Liu, Y. Feng, C. Zhang, Z.L. Wang, *Energy Environ. Sci.* 13 (2020) 277-285.
- 8 [16] H. Chen, Y. Song, X. Cheng, H. Zhang, *Nano Energy*. 56 (2019) 252-268.
- 9 [17] F. Huang, H. Yu, S. Xiang, J. Xue, H. Ming, C. Tao, N. Zhang, X. Fan, *ACS Appl. Mater. Interfaces*.
10 12 (2020) 3654-3660.
- 11 [18] T.G. Yun, J. Bae, A. Rothschild, I.D. Kim, *ACS Nano*. 13 (2019) 12703-12709.
- 12 [19] J. Shi, S. Liu, L. Zhang, B. Yang, L. Shu, Y. Yang, M. Ren, Y. Wang, J. Chen, W. Chen, Y. Chai, X.
13 Tao, *Adv. Mater.* 32 (2020) 1901958.
- 14 [20] J.W. Lee, S. Jung, T.W. Lee, J. Jo, H.Y. Chae, K. Choi, J.J. Kim, J.H. Lee, C. Yang, J.M. Baik, *Adv.*
15 *Energy Mater.* 9 (2019) 1901987.
- 16 [21] J. Xiong, H. Luo, D. Gao, X. Zhou, P. Cui, G. Thangavel, K. Parida, P.S. Lee, *Nano Energy*. 61 (2019)
17 584-593.
- 18 [22] H. Guo, J. Wan, H. Wu, H. Wang, L. Miao, Y. Song, H. Chen, M. Han, H. Zhang, *ACS Appl. Mater.*
19 *Interfaces*. 12 (2020) 22357-22364.
- 20 [23] J. Xiong, G. Thangavel, J. Wang, X. Zhou, P.S. Lee, *Sci. Adv.* 6 (2020) eabb4246.
- 21 [24] N. Zhang, F. Huang, S. Zhao, X. Lv, Y. Zhou, S. Xiang, S. Xu, Y. Li, G. Chen, C. Tao, Y. Nie, J. Chen,
22 X. Fan, *Matter*. 2 (2020) 1260-1269.
- 23 [25] J. Xiong, P. Cui, X. Chen, J. Wang, K. Parida, M.F. Lin, P.S. Lee, *Nat. Commun.* 9 (2018) 1-9.
- 24 [26] K. Meng, S. Zhao, Y. Zhou, Y. Wu, S. Zhang, Q. He, X. Wang, Z. Zhou, W. Fan, X. Tan, J. Yang, J.
25 Chen, *Matter*. 2 (2020) 896-907.
- 26 [27] J. Xiong, P.S. Lee, *Sci. Technol. Adv. Mater.* 20 (2019) 837-857.
- 27 [28] N. Zhang, Y. Li, S. Xiang, W. Guo, H. Zhang, C. Tao, S. Yang, X. Fan, *Nano Energy*. 72 (2020)
28 104664.

- 1 [29] Z. Lin, J. Yang, X. Li, Y. Wu, W. Wei, J. Liu, J. Chen, J. Yang, *Adv. Funct. Mater.* 28 (2018) 1704112.
- 2 [30] X. Pu, M. Liu, X. Chen, J. Sun, C. Du, Y. Zhang, J. Zhai, W. Hu, Z.L. Wang, *Sci. Adv.* 3 (2017)
3 e1700015.
- 4 [31] L. Zheng, S. Dong, J. Nie, S. Li, Z. Ren, X. Ma, X. Chen, H. Li, Z.L. Wang, *ACS Appl. Mater. Inter-*
5 *faces.* 11 (2019) 42504-42511.
- 6 [32] Y. Zou, P. Tan, B. Shi, H. Ouyang, D. Jiang, Z. Liu, H. Li, M. Yu, C. Wang, X. Qu, L. Zhao, Y. Fan,
7 Z.L. Wang, Z. Li, *Nat. Commun.* 10 (2019) 1-10.
- 8 [33] Y.C. Lai, Y.C. Hsiao, H.M. Wu, Z.L. Wang, *Adv. Sci.* 6 (2019) 1801883.
- 9 [34] Z. Li, M. Zhu, J. Shen, Q. Qiu, J. Yu, B. Ding, *Adv. Funct. Mater.* 30 (2020) 1908411.
- 10 [35] J. Zhao, W. Zhu, X. Wang, L. Liu, J. Yu, B. Ding, *ACS Nano.* 14 (2020) 1045-1054.
- 11 [36] V. Sencadas, C. Garvey, S. Mudie, J.J.K. Kirkensgaard, G. Gouadec, S. Hauser, *Nano Energy.* 66
12 (2019) 104106.
- 13 [37] J.Y. Cheong, M. Mafi, L. Benker, J. Zhu, M. Mader, C. Liang, H. Hou, S. Agarwal, I.D. Kim, A.
14 Greiner, *ACS Appl. Mater. Interfaces.* 12 (2020) 18002-18011.
- 15 [38] X. Wang, Y. Zhang, X. Zhang, Z. Huo, X. Li, M. Que, Z. Peng, H. Wang, C. Pan, *Adv. Mater.* 30
16 (2018) 1706738.
- 17 [39] X. Liang, T. Zhao, W. Jiang, X. Yu, Y. Hu, P. Zhu, H. Zheng, R. Sun, C.P. Wong, *Nano Energy.* 58
18 (2019) 508-516.
- 19 [40] A.R. Mule, B. Dudem, H. Patnam, S.A. Graham, J.S. Yu, *ACS Sustain. Chem. Eng.* 7 (2019)
20 16450-16458.
- 21 [41] Y. Liu, L. Wang, L. Zhao, K. Yao, Z. Xie, Y. Zi, X. Yu, *Adv. Electron. Mater.* 6 (2020) 1901174.
- 22 [42] J. Yu, X. Hou, J. He, M. Cui, C. Wang, W. Geng, J. Mu, B. Han, X. Chou, *Nano Energy.* 69 (2020)
23 104437.
- 24 [43] F. Liang, X.J. Zhao, H.Y. Li, Y.J. Fan, J.W. Cao, Z.L. Wang, G. Zhu, *Nano Energy.* 69 (2020) 104414.
- 25 [44] L. Zhu, X. Zhou, Y. Liu, Q. Fu, Highly Sensitive, *ACS Appl. Mater. Interfaces.* 11 (2019)
26 12968-12977.
- 27 [45] L. Liu, H.Y. Li, Y.J. Fan, Y.H. Chen, S.Y. Kuang, Z. Bin Li, Z.L. Wang, G. Zhu, *Small.* 15 (2019)
28 1900755.

- 1 [46] Y.J. Fan, X. Li, S.Y. Kuang, L. Zhang, Y.H. Chen, L. Liu, K. Zhang, S.W. Ma, F. Liang, T. Wu, Z.L.
2 Wang, G. Zhu, ACS Nano. 12 (2018) 9326-9332.
- 3 [47] Y. Guo, W. Zhou, L. Wang, Y. Dong, J. Yu, X. Li, B. Ding, ACS Appl. Bio Mater. 2 (2019) 5949-5956.
- 4 [48] N. Zheng, Y. Song, L. Wang, J. Gao, Y. Wang, X. Dong, Ind. Eng. Chem. Res. 58 (2019),
5 15470-15478.
- 6 [49] Y. Ertas, T. Uyar, Carbohydr. Polym. 177 (2017) 378-387.
- 7 [50] M. W. Matsen, F. S. Bates, Macromolecules. 29 (1996) 7641-7644.
- 8 [51] M. W. Matsen, F. S. Bates, Macromolecules. 29 (1996) 1091-1098.
- 9 [52] L. Wang, P.D. Topham, O.O. Mykhaylyk, H. Yu, A.J. Ryan, J.P.A. Fairclough, W. Bras, Macromol.
10 Rapid Commun. 36 (2015) 1437-1443.
- 11 [53] J. P. Lee, J. W. Lee, J. M. Baik, Micromachines. 9 (2018) 532.
- 12 [54] X. Yang, Y. Wang, X Qing, Sensors Actuators, A Phys. 299 (2019) 111579.
- 13 [55] H. Kang, H. Kim, S. Kim, H.J. Shin, S. Cheon, J.H. Huh, D.Y. Lee, S. Lee, S.W. Kim, J.H. Cho, Adv.
14 Funct. Mater. 26 (2016) 7717-7724.
- 15 [56] S. Oberoi, D. Sonawane, P. Kumar, Compos. Sci. Technol. 127 (2016) 185-192.
- 16 [57] S.M. Daghash, O.E. Ozbulut, Mater. Des. 111 (2016) 504-512.
- 17 [58] R. Menini, M. Farzaneh, Polym. Int. 51 (2008) 77-84.
- 18 [59] Y. Si, Z. Dong, L. Jiang, ACS Cent. Sci. 4 (2018) 1102-1112.
- 19 [60] J. Xue, T. Wu, Y. Dai, Y. Xia, Chemical Reviews. 119 (2019) 5298-5415.
- 20 [61] Y. Li, Z. Zhu, J. Yu, B. Ding, ACS Appl. Mater. Interfaces. 7 (2015) 13538-13546.
- 21 [62] J. Wang, G. Cai, S. Li, D. Gao, J. Xiong, P. S. Lee, Adv. Mater. 30 (2018) 1706157.
- 22 [63] Y. Yang, J. Han, J. Huang, J. Sun, Z. L. Wang, S. Seo, Q. Sun, Adv. Funct. Mater. 30 (2020)
23 201909652.
- 24 [64] C. Wu, T. W. Kim, J. H. Park, B. Koo, S. Sung, J. Shao, C. Zhang, Z. L. Wang, ACS Nano. 14 (2020)
25 1390-1398.
- 26 [65] Z. L. Wang, Nano Energy. 68 (2020) 104272.

27

28



1 **Mr. Yi Li** received his bachelor degree from Wuhan University in 2012. Now he a
2 Ph.D. candidate in the School of Electric Engineering and Automation, Wuhan
3 University. He is also a visiting graduate in the School of Materials Science and
4 Engineering, Nanyang Technological University. His research focus on SF₆ alter-
5 native gas, triboelectric nanogenerators and self-powered sensors for smart power
6 system.
7



8 **Dr. Jiaqing Xiong** received his Ph.D. from Soochow University in 2015. Now he is a
9 senior research fellow in the School of Materials Science and Engineering, Nanyang
10 Technological University. His research focuses on smart fibers/textiles, flexible and
11 wearable devices, and functional materials for self-powered systems and hu-
12 man-machine interface.



13 **Dr. Jian Lv** received his Ph.D in Material Science and Engineering at Xi'an Jiaotong
14 University in June 2019. During 2017-2019, he was a visiting graduate and then a re-
15 search associate at University of California, San Diego. He is currently a research fel-
16 low at the Nanyang Technological University, Singapore. His main research interests
17 involve the printed wearable and stretchable devices with the applications in energy
18 harvesting/storage and health care monitoring.
19
20
21
22



23 **Dr. Jian Chen** received his B.S. degree in Central South University in 2014, and his
24 Ph.D. degree in Condensed Matter Physics from University of Chinese Academy of
25 Sciences in 2019. Now he is a postdoctoral fellow in Nanyang Technological Univer-
26 sity. His research interests include triboelectric nanogenerators, self-powered systems
27 and soft robot.
28
29
30



31 **Mr. Dace Gao** received his B.Eng. from ZheJiang University in 2016. He is currently
32 a PhD student under the supervision of Prof. Lee Pooi See at Nanyang Technological
33 University. His research interests include additive manufacturing, soft electronics, and
34 soft robotics.
35
36
37



1 **Prof. Xiaoxing Zhang** received his Bachelor and Master degrees from Hubei University
2 of Technology, and Doctor degree from Chongqing University. He is currently a professor
3 of School of Electrical and Electronic Engineering, Hubei University of Technology. His
4 research focus in the online monitoring and fault diagnosis of high voltage electrical in-
5 sulation equipment, SF₆ alternative gases and gas sensors.
6

7



8 **Prof. Pooi See Lee** received her Ph.D. from National University of Singapore in 2002.
9 She joined the School of Materials Science and Engineering, Nanyang Technological
10 University as an Assistant Professor in 2004. She was promoted to tenured Associate
11 Professor in 2009 and full Professor in 2015. Her research focuses on nanomaterials for
12 energy and electronics applications, flexible and stretchable devices, electrochemical in-
13 spired devices, and human-machine interface. She received the National Research Foun-
14 dation Investigatorship Award and the Nanyang Research Excellence Award in 2016.
15