

# Can the mechanoreceptional setae of a feeding-current feeding copepod detect hydrodynamic disturbance induced by entrained free-floating prey?

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1 **Supplemental Information -- Can the mechanoreceptional setae of a**  
2 **feeding-current feeding copepod detect hydrodynamic disturbance**  
3 **induced by entrained free-floating prey?**

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11 Running head: Prey detection in feeding currents

12 Key Words: copepods, seta, mechanoreception, feeding-current feeding, prey detection,  
13 hydrodynamic sensitivity, setal deformation

## 14 *Detailed copepod model*

15 The geometry of our copepod model is based on copepods *Paracalanus parvus* and  
16 *Pseudocalanus sp.* in supplementary videos 1 and 3 of Tiselius et al. (2013). The copepod  
17 prosome of length  $L_b = 1$  mm is approximated to be two semi-ellipsoids attached to a cone-  
18 shaped urosome; the cephalosome is then extruded to allow the attachment of the cephalic  
19 appendages (Fig. S1). The stationary swimming legs are modeled as a prism intersecting with the  
20 prosome, while the centerline of the antennule with arc length  $L_{A1} = 1.097$  mm is fitted to a fifth-  
21 order polynomial. Figs. S1a,b show the geometrical parameters of the copepod model.

22 The feeding appendage geometries and beating patterns are modeled as follows.  
23 Morphological examination shows that the antennae, first maxillae, and mandibles are biramous  
24 (two branches) while the maxillipeds are uniramous (single branch); the distal segments of  
25 mandibles share a common proximal segment and are separated by a small angle (refer to fig. 2  
26 of Conway (2006)). We first determine the attachment points of appendage roots from Tiselius et  
27 al. (2013), which are represented by the longitudinal distance measured from the head tip  $l$  and  
28 lateral distance from the sagittal plane  $w$  (refer to Fig. S1a insert, and also see the “ $l$ ” and “ $w$ ”  
29 columns in Table S1). To model the appendage geometries, we then approximate the first  
30 maxilla to be a cylinder with one degree of freedom only (see Fig. S1c). The distal segments of  
31 the mandible are close to each other, so we treat them as one branch. Therefore, we approximate  
32 each branch of antenna, mandible and maxilliped as a rigid circular frustum (see the “root  
33 diameter” column in Table S1). The setules and setae on the feeding appendages are not  
34 explicitly accounted for in the hydrodynamic model; instead, the root diameters of all  
35 appendages are 1.5 times the values obtained from the image analysis.

36 We obtain the projected motions of the antennae, mandibles, first maxillae and maxillipeds  
37 from supporting video 1 of Tiselius et al. (2013), as these four pairs of appendages are involved  
38 in generating the actual feeding current (Tiselius et al. 2013; van Duren and Videler 2003). For  
39 each appendage, in every video frame we determine the angles from the copepod's transverse  
40 plane to the proximal and distal segments,  $\theta_1$  and  $\theta_2$  (see Fig. S1a inset), respectively. We  
41 perform a fast Fourier transform on all  $\theta_1$  and  $\theta_2$  to express their time-dependence analytically by  
42 using the first two leading terms (see the “angle” column in Table S1). The last pair of feeding  
43 appendages, second maxillae, is found to stay almost stationary (Gill and Poulet 1986) and only  
44 move occasionally to handle food particles upon detection (van Duren and Videler 2003);  
45 therefore, we neglect the presence of the second maxillae in our model.

46 To recover the three dimensional beating patterns of the feeding appendages, we find the  
47 mean projected lengths of the four feeding appendages, antennae, mandibles, first maxillae, and  
48 maxillipeds, from supporting video 1 of Tiselius et al. (2013), and the corresponding projection  
49 angle  $\alpha$  in Fig. S1a inset, according to the copepod schematics as shown in fig. 2 of Koehl and  
50 Strickler (1981). Table S1 shows the true lengths and  $\alpha$  of all feeding appendage segments.

## 51 *Immersed boundary method*

### 52 **Governing equations**

53 The feeding current and prey entrainment are governed by the unsteady and incompressible  
54 Navier-Stokes equations

$$55 \quad \rho \left[ \partial_t \mathbf{u}(\mathbf{x}, t) + \mathbf{u}(\mathbf{x}, t) \cdot \nabla \mathbf{u}(\mathbf{x}, t) \right] = -\nabla p(\mathbf{x}, t) + \mu \nabla^2 \mathbf{u}(\mathbf{x}, t) + \mathbf{f}_b(\mathbf{x}, t), \quad (\text{S1})$$

$$56 \quad \nabla \cdot \mathbf{u}(\mathbf{x}, t) = 0, \quad (\text{S2})$$

57 where  $\rho = 10^3 \text{ kg/m}^3$  is the fluid density;  $\mu = 10^{-3} \text{ Ns/m}^2$  is the viscosity;  $\mathbf{u}$ ,  $p$ ,  $\mathbf{f}_b$  are the fluid  
58 velocity, pressure, and force at position  $\mathbf{x}$  and time  $t$ , respectively.

59 Due to the no-slip boundary condition, the fluid velocity at the surfaces of the copepod and  
60 its appendages must be equal to the velocity of those surfaces. Owing to the complexity of the  
61 feeding appendages' beating strokes, it is useful to apply the immersed boundary (IB) method to  
62 account for the no-slip boundary condition (Peskin 1972; Peskin 2002), which requires forces to  
63 be exerted on the fluid at the surfaces. The forces and the no-slip boundary condition in the IB  
64 framework are expressed as

$$65 \quad \mathbf{f}_b(\mathbf{x}, t) = \int_U \mathbf{F}(\mathbf{s}, t) \delta(\mathbf{x} - \mathbf{X}(\mathbf{s}, t)) d\mathbf{s}, \quad (\text{S3})$$

$$66 \quad \partial_t \mathbf{X}(\mathbf{s}, t) = \int_\Omega \mathbf{u}(\mathbf{x}, t) \delta(\mathbf{x} - \mathbf{X}(\mathbf{s}, t)) d\mathbf{x}, \quad (\text{S4})$$

67 where  $\Omega$  denotes the space occupied by the immersed copepod;  $\mathbf{F}(\mathbf{s}, t)$  and  $\mathbf{X}(\mathbf{s}, t)$  are the force  
68 density applied by the copepod to the fluid and its physical position of the material point  $\mathbf{s} \in \Omega$  at  
69 time  $t$ , respectively;  $\delta(\mathbf{x})$  is the three-dimensional Dirac delta function in our problem.

## 70 **Mesh independence test**

71 The spatial and temporal distribution of the feeding current due to a tethered feeding-current  
72 feeding copepod is calculated by using the constraint IB version (Bhalla et al. 2013) of IBAMR  
73 (<https://ibamr.github.io/>, last accessed on July 23, 2021). In our simulation, we set the origin of  
74 the Cartesian coordinate to be at the center of a cubical computational domain of length  $L = 10$   
75 mm. We then place the copepod of prosome length  $L_b = 1$  mm into the domain such that at time  $t$   
76  $= 0$ , the copepod's center of mass coincides with the origin, its anterior-posterior direction along  
77 the positive  $x$ -axis and its ventral-dorsal direction along the positive  $z$ -axis. IBAMR discretizes  
78 the computational domain into Cartesian grids and refines the grids if necessary. As a result, the  
79 coarsest grids are distributed around the boundaries of the computational domain, while the  
80 finest grids enclose the tethered copepod and prey. There are three variables that determine the

81 total number of grids: first, the number of coarsest grids per length  $N$  which controls the size of  
82 the coarsest grid  $dx^1 = L/N$ , second, the refinement ratio  $R_{\text{ref}}^i$  which controls how each coarse  
83 grid is divided into the next finer grid with size  $dx^{i+1} = dx^i / R_{\text{ref}}^i$ , and last, the refinement level  
84  $n_{\text{ref}}$ , which determines the upper bound of the positive integer  $i$ . The mesh refinement is  
85 automatically determined by the IBAMR software, and hence the grid may vary between each  
86 time step.

87 The mesh independence test is performed by comparing the velocities at three sample points  
88 in the computational domain as the variables  $(N, R_{\text{ref}}^i, n_{\text{ref}})$  are varied: the tips of the proximal  
89 and distal setae on the left antennule, and Point D close to the beating appendages at  $\mathbf{x}/L_b = [0, 0,$   
90  $-0.5]$ . The mesh independence test is conducted by setting the maximum time step  $\Delta t_{\text{max}}/T = 5 \times$   
91  $10^{-4}$  so that the convective Courant-Friedrichs-Lewy number is not more than 0.05, where the  
92 period of the beating stroke  $T = 1/30$  s. In Fig. S2, we show the magnitudes of the flow velocities  
93 at the end of the first beating period,  $|\mathbf{u}(\mathbf{x}, T)|$ , for the variables  $N$ ,  $R_{\text{ref}}^i$  and  $n_{\text{ref}}$ . We consider the  
94 flow velocity computed using a certain grid to be converged if  $|\mathbf{u}(\mathbf{x}, T)|$  at the three sample points  
95 are within 5% of those at the finest grid. For all three points, we find that the flow velocities are  
96 converged at  $N = 20$ ,  $n_{\text{ref}} = 3$  and  $R_{\text{ref}}^i = 4$ .

## 97 **Validation of numerical model**

98 We validate our numerical model by comparing the time-averaged feeding current with the  
99 experiment of Fields and Yen (1997). The experiment tethered a *Euchaeta rimana* female ( $L_b =$   
100  $2.5$  mm), and traced the time-dependent positions of  $20 \mu\text{m}$  polystyrene beads entrained in the  
101 feeding current. The trajectories of the beads and spatial distribution of the magnitude of the  
102 feeding current at the antennule region are shown in figs. 3 and 4 of Fields and Yen (1997),

103 respectively. The beating frequency of the feeding appendages is not reported but we estimate it  
 104 to be 33 Hz based on the linear regression of the limb paddling frequency during cruise  
 105 swimming (see figs. 3 and 4 of Svetlichny et al. (2020)).

106 In Fig. S3, we show the oscillatory nature of the feeding current,  $\mathbf{u}(\mathbf{x}, t)$ , by plotting it (in the  
 107 absence of prey) in a plane coincident with the centerlines of the antennule at 5 selected time  
 108 frames during the  $N$ -th beating stroke.

109 We decompose the feeding current during one beating stroke into time-averaged and  
 110 oscillatory components,

$$111 \quad \mathbf{u}(\mathbf{x}, t) = \mathbf{u}_{\text{avg}}(\mathbf{x}, NT) + \mathbf{u}_{\text{osc}}(\mathbf{x}, t), \quad (\text{S5})$$

112 where  $\mathbf{u}_{\text{avg}} = (1/T) \int_{(N-1)T}^{NT} \mathbf{u} dt$  is the time-averaged feeding current at the  $N$ -th beating stroke, and

113  $\mathbf{u}_{\text{osc}}$  represents the oscillatory velocity component of the feeding current. In Fig. S4a, we plot the  
 114 time-averaged feeding current in our model, and find it is similar to that in fig. 3 of Fields and  
 115 Yen (1997), in which the flow contracts before reaching the copepod body, and diverges after  
 116 passing through. The flow pattern is similar to that due to a Stokeslet, which is consistent with  
 117 the prediction of Visser (2001) and measurements in Malkiel et al. (2003) and Catton et al.  
 118 (2007). The largest average velocity is around the feeding appendages, and it decays as the  
 119 distance from the copepod increases. The average velocity shows two local maxima (1.8 mm/s)  
 120 in front of the proximal region of the antennule, and becomes significantly smaller in the distal  
 121 region of the antennule (0.15 mm/s). In comparison, experiments reported average velocities at  
 122 the proximal and distal regions of the antennule are 8 mm/s and 1 mm/s, respectively (see fig. 4  
 123 of Fields and Yen (1997)). The experimental velocities are expected to be larger than our  
 124 numerical velocities, since *Euchaeta rimana* ( $L_b = 2.5$  mm) is larger than our model copepod ( $L_b$   
 125 = 1 mm), and velocity scale is set by the product of the prosome length  $L_b$  and beating frequency  $f$ .

126 If we normalize the experimental and numerical velocities by this quantity ( $L_{bf}$ ), the  
127 experimental velocities at the proximal and distal of the antennule are of the same order of  
128 magnitude, but about 1.6 and 2.4 times larger than the corresponding numerical values,  
129 respectively. Note that we chose the enlarged effective radii of the feeding appendages to make  
130 these normalized velocities as close as possible. We attribute the errors in the calculated feeding  
131 current to the approximations made in our numerical model: first, the feeding appendage  
132 geometries and motion may not be captured accurately, second, we assumed that the antennae  
133 are motionless, and third, the use of effective radii for appendages instead of modeling the fine  
134 structure of setae and setules on the appendages. In Fig. S4b, we plot the peak-to-peak magnitude  
135 of the oscillatory component of the feeding current without the presence of the prey, which is  
136 defined as the difference between the two extrema of the magnitude of the feeding current in one  
137 beating cycle.

### 138 *Steady state test*

139 We evaluate the feeding current velocities at the three sample points to estimate how many  
140 beating cycles are required for the bending flows across the setae to reach 98% of the steady  
141 state value. We first consider the feeding current velocity without the presence of the prey,  
142  $|\mathbf{u}(\mathbf{x},t)|$ , at Point D. The solid line in Fig. S5a plots the magnitude of its time-averaged velocity  
143 component over the first 100 beating cycles, while the vertical bar represents the range of the  
144 oscillatory velocity component. We find that the time-averaged feeding current at Point D  
145 requires 4 beating cycles to reach 98% of its steady state value. In Fig. S5b (Fig. S5c), we show  
146 the magnitudes of the feeding current at the tips of the proximal (distal) setae. The solid line in  
147 each panel represents the corresponding time-averaged velocity component, while the vertical  
148 bar represents the range of oscillation. We find that it requires the time-averaged feeding current

149 about 4 and 57 beating cycles for the flow across the proximal and distal setae to reach 98% of  
150 their corresponding steady-state values, respectively. This is due to the fact that the feeding  
151 current takes longer time to reach steady state at larger distances from the feeding appendages.  
152 Therefore, we use the feeding current at  $t/T = 60$  to evaluate the steady-state bending flows at all  
153 setae on the antennule and feeding appendages.

#### 154 ***Bending Flow across the Setae on the Antennule without the Presence of the Prey***

155 In Fig. S6, we plot the  $x$ ,  $y$  and  $z$  components of the steady-state  $\Delta\mathbf{u}(s,t)$  across the distal and  
156 proximal setae on the antennule at selected times over one beating cycle. It is apparent that the  
157 bending flow across these setae is highly oscillatory, which are generated by oscillatory  
158 movement of the feeding appendages.

#### 159 ***Oscillatory component of the bending flow***

160 In Fig. S7a (Fig. S7b), we plot the oscillatory component of the bending flow,  $\Delta\mathbf{u}_{\text{osc}}(s,t)$ ,  
161 across the distal (proximal) seta at the number of beating cycle when the free-floating prey  
162 initiated from Point B (Point C) is generates the largest time-averaged feeding current.

#### 163 ***Numerical scheme for setal deformation***

164 We define the physical coordinate of the setal centerline to be  $\mathbf{X}(s,t)$ , where  $s$  is a  
165 Lagrangian parameter along the centerline of the seta starting from the setal root;  $L_{\text{seta}}$  is the  
166 setal length. Our numerical scheme discretizes the centerline of the seta into  $M$  rigid segments  
167 with equal arclength  $\Delta s = L_{\text{seta}}/M$ . We express the centerline coordinate of the  $m$ -th segment  
168 center as  $s_{m+1/2} = (m + 1/2)\Delta s$  and the segment endpoints as  $s_m = m\Delta s$  and  $s_{m+1} = (m + 1)\Delta s$ , for  $m$   
169  $= 0, 1, \dots, M - 1$ . In the discretized form, we use  $\mathbf{X}_m$  and  $\mathbf{X}_{m+1/2}$  to represent the physical

170 coordinate of the setal centerline at the corresponding  $m$ -th segment endpoint or center,  
 171 respectively.

## 172 **Method of regularized Stokeslets**

173 Our implementation of the method of regularized Stokeslets (MRS) is similar to that  
 174 described in Hyon et al. (2012) and Martindale et al. (2016). We place a total number of  $N$   
 175 regularized Stokeslets uniformly on the surface of the seta. To do so, we first divide each  
 176 segment by equally spaced circular cross sections of radius  $r_{\text{seta}}$ . For each cross section, we place  
 177 a total number of  $P$  regularized Stokeslets equally spaced along the perimeter of each cross  
 178 section such that the arc distance between successive regularized Stokeslets  $2\pi r_{\text{seta}}/P$  is  
 179 approximately the same as the distance between successive cross sections (see Fig. 8). The  
 180 regularized Stokeslets in the successive cross sections are staggered in such a way that the  
 181 successive cross sections are rotated around the centerline axis by an angle of  $\pi/P$ . After rotation,  
 182 the physical coordinates of the regularized stokeslets are denoted by  $X_n$ , for  $n = 1, 2, \dots, N$ .

183 We apply the MRS to explicitly evaluate the velocity at the  $m$ -th segment center,  $\mathbf{v}_{m+1/2} =$   
 184  $\mathbf{v}(\mathbf{X}_{m+1/2}, t)$ , which is a sum of the velocity due to the background flow and that due to a linear  
 185 superposition of the forces due to the regularized Stokeslets:

$$186 \quad \mathbf{v}_{m+1/2} = \Delta \mathbf{u}(\mathbf{X}_{m+1/2}, t) + \sum_{n=0}^N \mathbf{S}(\mathbf{X}_{m+1/2}, X_n, \delta) F_n(t), \quad (\text{S6})$$

187 where  $\Delta \mathbf{u}$  is the bending flow velocity obtained from IBAMR with reference to that at the setal  
 188 root,  $F_n$  is the regularized Stokeslet force centered at  $X_n$  at time  $t$ ,  $\mathbf{S}(\mathbf{X}_{m+1/2}, X_n, \delta)$  is the  
 189 regularized Stokeslet kernel given by Eq. 10(b) in the work of Cortez et al. (2005), and  $\delta$  is the  
 190 regularization parameter which is in the same order of magnitude as  $2\pi r_{\text{seta}}/P$ .

## 191 **Inextensible Kirchhoff rod theory**

192 Our implementation of the inextensible Kirchhoff Rod Theory (KRT) is similar to that  
 193 described in Jabbarzadeh and Fu (2020). The inextensible constraint imposed on the seta  
 194 enforces zero longitudinal deformation of the seta, which implies that

$$195 \quad |\partial_s \mathbf{X}| = 1. \quad (\text{S7})$$

196 This is implemented in our numerical model by assuming all setal segments are all rigid; the  
 197 transverse deformation of the seta is captured by the angular displacements of the torsional  
 198 springs connecting adjacent segments (see Fig. S8).

199 To solve for the internal force and torque exerted on the seta, we first express the  
 200 hydrodynamic force and torque per length exerted at the setal centerline, denoted by  $\mathbf{f}(s,t)$  and  
 201  $\mathbf{n}(s,t)$  in Eqs. 2 and 3 in the main text, in terms of  $\mathbf{F}_n$ . In discretized form, we have

$$202 \quad \mathbf{f}_{m+1/2} = \frac{1}{\Delta s} \sum_{n=mN/M+1}^{(m+1)N/M} \mathbf{F}_n, \quad (\text{S8})$$

$$203 \quad \mathbf{n}_{m+1/2} = \frac{1}{\Delta s} \sum_{n=mN/M+1}^{(m+1)N/M} (\mathbf{X}_n - \mathbf{X}_{m+1/2}) \times \mathbf{F}_n, \quad (\text{S9})$$

204 where  $\mathbf{f}_{m+1/2} = \mathbf{f}(\mathbf{X}_{m+1/2}, t)$  and  $\mathbf{n}_{m+1/2} = \mathbf{n}(\mathbf{X}_{m+1/2}, t)$  represents the force and torque per unit length at  
 205 the  $m$ -th segment center, respectively. We further use a set of orthonormal basis vectors,  $\mathbf{d}_i(s,t) \in$   
 206  $\mathbb{R}^3$  for  $i = 1, 2, 3$ , to express the orientation of the setal centerline, and to further relate it with  
 207 torsion of the cross sections. The unit tangential vector along the setal centerline can be  
 208 expressed as

$$209 \quad \mathbf{d}_3 = \partial_s \mathbf{X} / |\partial_s \mathbf{X}|. \quad (\text{S10})$$

210 This allows us to use the discretized form of the Kirchhoff Rod equations (Eqs. 2 and 3 in the  
 211 main text) to further relate  $\mathbf{f}_{m+1/2}$  and  $\mathbf{n}_{m+1/2}$  with the internal force and torque at the segment ends  
 212 by using

213 
$$\mathbf{F}_m = (\mathbf{f}_{m-1/2} - \mathbf{f}_{m+1/2}) \Delta s, \quad (\text{S11})$$

214 
$$\mathbf{N}_m = (\mathbf{n}_{m-1/2} - \mathbf{n}_{m+1/2}) \Delta s - (\mathbf{d}_{m-1/2,3} \times \mathbf{f}_{m-1/2} + \mathbf{d}_{m+1/2,3} \times \mathbf{f}_{m+1/2}) \Delta s^2 / 2, \quad (\text{S12})$$

215 where

216 
$$\mathbf{F}_m = \sum_{i=1}^3 F_{m,i} \mathbf{d}_{m,i}, \quad (\text{S13})$$

217 
$$\mathbf{f}_{m\pm 1/2} = \sum_{i=1}^3 f_{m\pm 1/2,i} \mathbf{d}_{m\pm 1/2,i}, \quad (\text{S14})$$

218 
$$\mathbf{N}_m = \sum_{i=1}^3 N_{m,i} \mathbf{d}_{m,i}, \quad (\text{S15})$$

219 
$$\mathbf{n}_{m\pm 1/2} = \sum_{i=1}^3 n_{m\pm 1/2,i} \mathbf{d}_{m\pm 1/2,i}. \quad (\text{S16})$$

220 We then use the rigid body constraint to express the velocities of the material points on the  
 221 setal surface,  $\mathbf{v}_n = \mathbf{v}(\mathbf{X}_n, t)$ , in terms of the translational and rotational velocities at the  $m$ -th  
 222 segment,

223 
$$\mathbf{v}_n = \mathbf{V}_{m+1/2} + \mathbf{\Omega}_{m+1/2} \times (\mathbf{X}_n - \mathbf{X}_{m+1/2}), \quad (\text{S17})$$

224 for  $mN / M + 1 \leq n \leq (m+1)N / M$ . We further express  $\mathbf{\Omega}_{m+1/2}$  in terms of  $\mathbf{\Omega}_{1/2}$  and  $\mathbf{V}_{m+1/2}$ . To do  
 225 so, we substitute Eq. (S7) into Eq. (S10), and differentiate the latter with respect to time, leading  
 226 to

227 
$$\frac{\partial \mathbf{V}(s, t)}{\partial s} = \mathbf{\Omega}(s, t) \times \mathbf{d}_3(s, t). \quad (\text{S18})$$

228 The discretized form of Eq. (S18) allows us to use

229 
$$\mathbf{V}_{m+1} - \mathbf{V}_m = \mathbf{\Omega}_{m+1/2} \times (\mathbf{X}_{m+1} - \mathbf{X}_m) \quad (\text{S19})$$

230 to relate  $\mathbf{\Omega}_{m+1/2}$  to the difference in the velocities between the two endpoints of the  $m$ -th segment,  
 231 and

232 
$$\mathbf{V}_{m\pm 1/2} - \mathbf{V}_m = \boldsymbol{\Omega}_{m+1/2} \times (\mathbf{X}_{m\pm 1/2} - \mathbf{X}_m) \quad (\text{S20})$$

233 to relate  $\boldsymbol{\Omega}_{m+1/2}$  to the difference in the velocities between the  $m$ -th segment center and either  
 234 endpoint.

235 **Forward time scheme**

236 We adopt a forward time scheme, which utilizes the setal shape and orientation at the time  
 237 step  $t = i\Delta t$ , for  $i = 0, 1, 2, \dots$ , to solve for centerline velocity of the seta, and then update the  
 238 setal shape at the following time step  $t = (i + 1)\Delta t$ .

239 To do so, we first find the hydrodynamic torque,  $\mathbf{N}_1, \mathbf{N}_2, \dots, \mathbf{N}_{M-1}$ , based on the setal shape  
 240 at the current time step,  $t = i\Delta t$ . This can be achieved by applying the discretized form of the  
 241 constitutive equation for the Kirchhoff rod model (Eqs. 4 to 6 in the main text):

242 
$$N_{m,1} = EI \left( \frac{\mathbf{d}_{m+1/2,2} - \mathbf{d}_{m-1/2,2}}{\Delta s} \cdot \mathbf{d}_{m,3} \right), \quad (\text{S21})$$

243 
$$N_{m,2} = EI \left( \frac{\mathbf{d}_{m+1/2,3} - \mathbf{d}_{m-1/2,3}}{\Delta s} \cdot \mathbf{d}_{m,1} \right), \quad (\text{S22})$$

244 
$$N_{m,3} = GJ \left( \frac{\mathbf{d}_{m+1/2,1} - \mathbf{d}_{m-1/2,1}}{\Delta s} \cdot \mathbf{d}_{m,2} \right), \quad (\text{S23})$$

245 where  $E$  is the Young's modulus;  $I = \pi r_{\text{seta}}^4/4$  and  $J = \pi r_{\text{seta}}^4/2$  are the planar and polar second  
 246 moment of the seta, respectively. The bending modulus  $G = E/[2(1 + \nu)]$ , where the Poisson's  
 247 ratio  $\nu$  is assumed to be 0.3.

248 Second, we couple the MRS and KRT and solve Eqs. (S6), (S8), (S9), (S11), (S12), (S17),  
 249 (S19) and (S20) as a linear system by using the internal torque  $\mathbf{N}_m$  obtained from Eqs. (S21) to  
 250 (S23) and the boundary conditions that the setal root is stationary and clamped ( $\mathbf{V}_{1/2} = \boldsymbol{\Omega}_{1/2} = \mathbf{0}$ )  
 251 and the setal tip is force- and moment-free ( $\mathbf{F}_M = \mathbf{N}_M = \mathbf{0}$ ) into the linear system. This allows us

252 to obtain the force and torque at the setal root,  $\mathbf{F}_0$  and  $\mathbf{N}_0$ , and the translational and rotational  
 253 velocities at the segment centers,  $\mathbf{V}_{m+1/2}$  and  $\mathbf{\Omega}_{m+1/2}$ .

254 Last, we update the setal shape and orientation at the following time step,  $t = (i + 1)\Delta t$ , by  
 255 using

$$256 \quad \mathbf{X}_{m+1/2}^{j+1} = \mathbf{X}_{m+1/2}^j + \mathbf{V}_{m+1/2}^j \Delta t, \quad (\text{S24})$$

$$257 \quad \mathbf{d}_{m+1/2,i}^{j+1} = R \left( \frac{\mathbf{\Omega}_{m+1/2}^j}{|\mathbf{\Omega}_{m+1/2}^j|}, |\mathbf{\Omega}_{m+1/2}^j| \Delta t \right) \mathbf{d}_{m+1/2,i}^j, \quad (\text{S25})$$

258 where  $R(\mathbf{e}, \theta)$  is the rotational matrix that depends on the rotational axis  $\mathbf{e}$  and rotational angle  $\theta$ .  
 259  $R(\mathbf{e}, \theta)$  is explicitly given by Eq. 36 in the work of Olson et al. (2013), and expressed as

$$260 \quad R(\mathbf{e}, \theta) = (\cos \theta) I + (1 - \cos \theta) \mathbf{e} \mathbf{e}^T + (\sin \theta) (\mathbf{e} \times), \quad (\text{S26})$$

261 where  $I \in \mathbb{R}^{3 \times 3}$  is an identity matrix, and for any vector  $\mathbf{d}$ ,  $(\mathbf{e} \times) \mathbf{d} = \mathbf{e} \times \mathbf{d}$ . The orthonormal basis  
 262 vectors at the segment endpoints are updated in such a way that

$$263 \quad \mathbf{d}_{m,i} = \begin{cases} \mathbf{d}_{1/2,i}, & \text{if } m = 0 \\ \mathbf{d}_{M-1/2,i}, & \text{if } m = M \\ \sqrt{\mathbf{A}} \mathbf{d}_{m-1/2,i}, & \text{if } m = 1, 2, \dots, M-1 \end{cases}, \quad (\text{S27})$$

264 where  $\mathbf{A} = \sum_{i=1}^3 \mathbf{d}_{m+1/2,i} (\mathbf{d}_{m-1/2,i})^T$ , and  $\sqrt{\mathbf{A}}$  is the square root of  $\mathbf{A}$ .

265 A convergence test was performed on a seta of length  $L_{\text{seta}} = 200 \mu\text{m}$ , radius  $r_{\text{seta}} = 1 \mu\text{m}$  and  
 266 Young's modulus  $E = 10^7 \text{ N/m}^2$ , which is subjected to a background shear flow  
 267  $\Delta \mathbf{u} = \dot{\epsilon} s \mathbf{d}_{0,2} \sin(2\pi ft)$ , where the frequency  $f = 30 \text{ Hz}$ , and the shear rate  $\dot{\epsilon} = 1 \text{ s}^{-1}$ . We note that  
 268 the parts that take most runtime in each time step are the linear solves implied by the matrix  
 269 inverse of the regularized Stokeslet kernel,  $\sum_{i=0}^N \mathbf{S}(\mathbf{X}_{m+1/2}, \mathbf{X}_i, \delta)$ , as shown in Eq. (S6). Here we  
 270 adopt the numerical framework that is stated in the ‘‘partial updating of hydrodynamic interaction’’

271 section in Jabbarzadeh and Fu (2020). In short, the kernel is recalculated only if the maximum  
272 difference between  $\mathbf{X}^j$  and  $\mathbf{X}^{j'}$  is larger than a prescribed threshold,

$$273 \quad \max(|\mathbf{X}^j - \mathbf{X}^{j'}|) > Cr_{\text{seta}}, \quad (\text{S28})$$

274 where  $\mathbf{X}^j$  represents the setal displacement at last time step that the kernel is updated, and  $C$  is a  
275 dimensionless constant to be determined in the convergence test. We set the setal deformation to  
276 be convergent if the maximum difference in the setal root curvature at selected  $(M, \Delta t, C)$  and the  
277 finest discretization level used in our numerics ( $M = 100, \Delta t = 4 \times 10^{-7}/f, C = 4 \times 10^{-4}$ ) is less  
278 than 5%. The convergence test results show that for  $\delta = 2\pi r_{\text{seta}}/(3P)$  and  $P = 12$ , the magnitude  
279 of the root curvature converges when  $\Delta t = 2 \times 10^{-6}/f$  and  $C = 0.4$ .

280

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322

323 Table S1. Hydrodynamic characteristics of the cephalic appendages – antennules (A1), antennae (A2), mandibles (Md), first maxillae  
 324 (Mx1), and maxillipeds (Mxp) – of copepod model

Appendage	Root diameter (mm) <sup>a</sup>	Tip diameter (mm) <sup>b</sup>	<i>l</i> (mm)	<i>w</i> (mm)	Segment	Length (mm) <sup>c</sup>	$\alpha$ (deg) <sup>d</sup>		Angle (rad) <sup>e</sup>
							endopod	exopod	
A1	0.062	0.022	0.051	0.031	–	1.097	–	–	–
A2	0.076	0.101	0.181	0.077	Proximal	0.184	36	64	$\theta_1 = +0.449 + 0.614 \cos(2\pi ft - 2.351)$
					Distal	0.152	–	–	$\theta_2 = -0.217 + 0.656 \cos(2\pi ft + 2.900)$
Md <sup>f</sup>	0.070	0.093	0.269	0.070	Proximal	0.111	80		$\theta_1 = +0.344 + 0.581 \cos(2\pi ft - 1.410)$
					Distal	0.162	–		$\theta_2 = -0.307 + 0.640 \cos(2\pi ft - 1.772)$
Mx1	0.050	0.050	0.319	0.066	–	0.179	10		$\theta_1 = +0.361 + 0.527 \cos(2\pi ft - 0.724)$
Mxp	0.064	0.085	0.476	0.053	Proximal	0.223	21		$\theta_1 = +0.094 + 0.328 \cos(2\pi ft + 0.876)$
					Distal	0.157	–		$\theta_2 = -5.267 + 0.527 \cos(2\pi ft + 1.171)$

325 <sup>a</sup> The diameter of appendage at its most proximal cross-section.

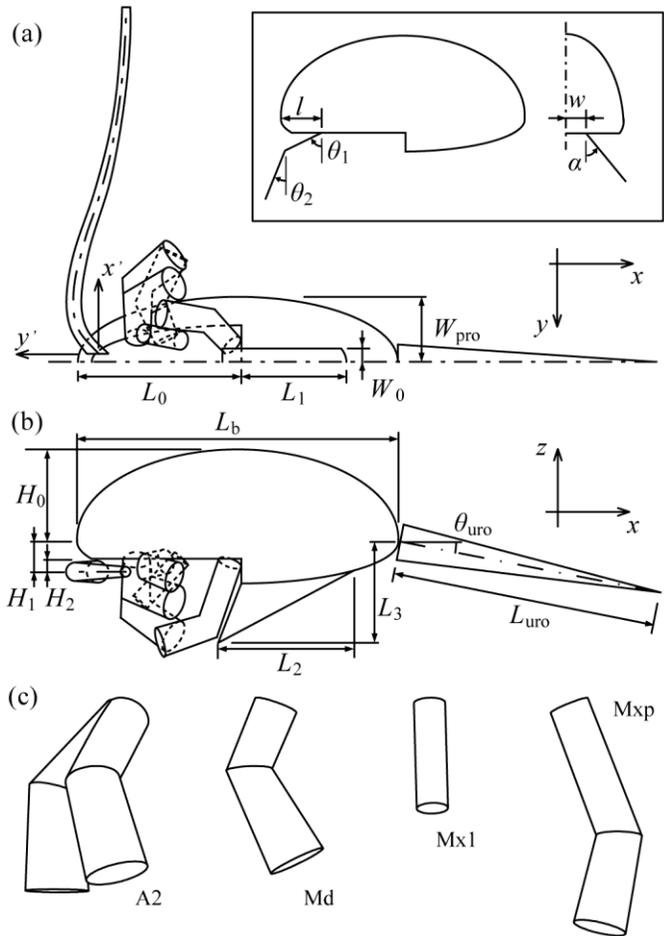
326 <sup>b</sup> The diameter of appendage at its most distal cross-section.

327 <sup>c</sup> The axial length (true length) of the appendage segment.

328 <sup>d</sup> Positive  $\alpha$  follows the arrow direction in Fig. S1a inset.

329 <sup>e</sup> The “Angle” represents  $\theta_1$  and  $\theta_2$  in Fig. S1a inset for proximal and distal segments, respectively;  $f$  is the beating frequency;  $t$  is the  
 330 time. Positive  $\theta_1$  and  $\theta_2$  follow the arrow directions in Fig. 1a inset.

331 <sup>f</sup> The biramous Md is simplified to be uniramous (single branch) with a distal segment attached to a proximal segment.



333

334 Fig. S1. (a) Ventral-dorsal and (b) lateral views of the feeding-current feeding copepod model.

335 The cone-shaped urosome is attached to the prosome composing of two semi-ellipsoids. The

336 ventral semi-ellipsoid is extruded for the attachment of cephalic appendages which from left to

337 right are the antennules (A1), antennae, mandibles, first maxillae, and maxillipeds. The

338 swimming legs are modeled as a prism intersecting with the prosome. (c) The schematics of the

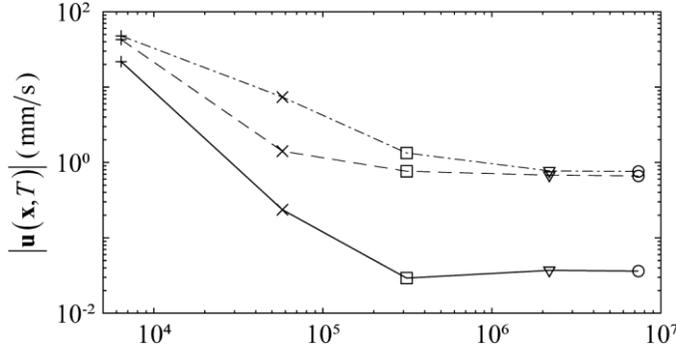
339 four feeding appendages in our model. The antenna is treated as two separated branches,

340 mandible, first maxilla and maxilliped as one branch. The left and right insets are schematics

341 illustrating the position of the attachment point  $[l, w]$ , longitudinal angular displacement  $[\theta_1, \theta_2]$ ,

342 and lateral angular displacement  $\alpha$ , of the cephalic appendages. The coordinate of the A1

343 centerline in the body-fixed frame is defined by  $y' = 1.704(x')^5 - 5.739(x')^4 + 7.519(x')^3 -$   
344  $4.550(x')^2 + 0.967x'$ , where both  $x'$  and  $y'$  are in units of mm. The prosome height is 0.399 mm,  
345 the base diameter of urosome is 0.097 mm and the other dimensions are:  $L_b = 1.000$  mm,  $L_{uro} =$   
346  $0.840$  mm,  $L_0 = 0.505$  mm,  $L_1 = 0.344$  mm,  $L_2 = 0.409$  mm,  $L_3 = 0.301$  mm,  $W_b = 0.200$  mm,  $W_0 =$   
347  $0.045$  mm,  $H_0 = 0.278$  mm,  $H_1 = 0.090$  mm,  $H_2 = 0.031$  mm and  $\theta_{uro} = 0.190$  rad.



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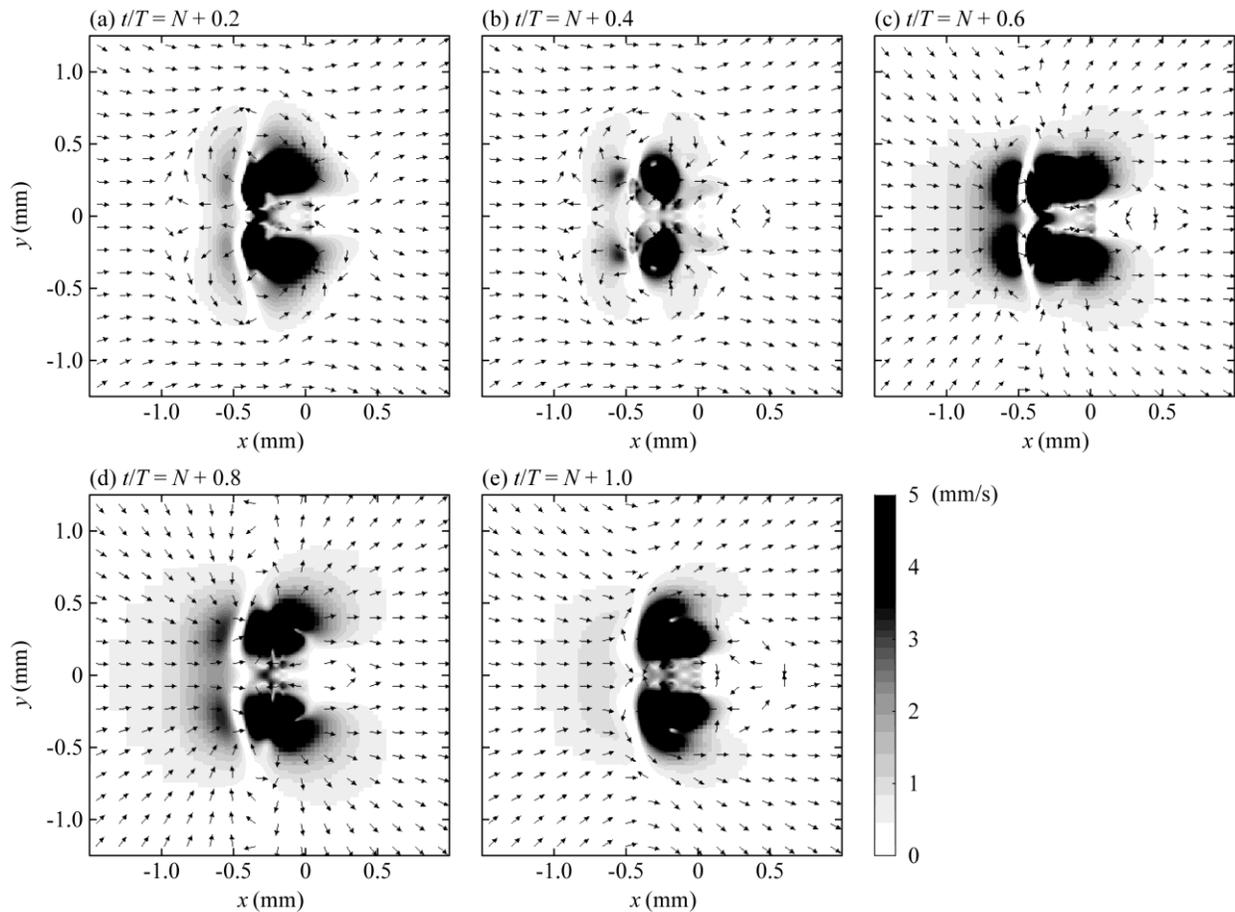
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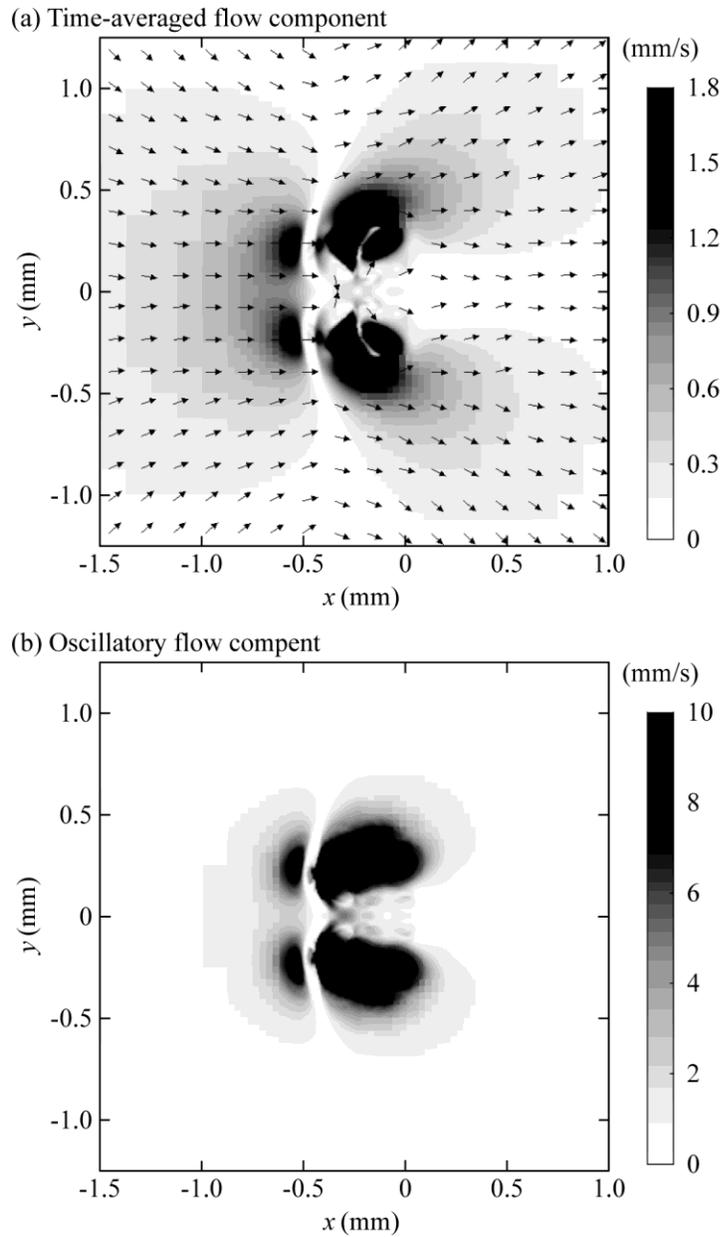
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Fig. S2. Magnitude of the feeding current velocity  $|\mathbf{u}(\mathbf{x}, t)|$  as a function of the total number of grid points at the end of the first beating period,  $t = T$ . The solid, dashed, dash-dotted and dotted lines represent the velocity at the distal setal tip, proximal setal tip, and Point D, respectively. The plus (+) symbols denote the number of grids when the number of coarsest grids per length  $N = 20$  and there is no mesh refinement. The cross ( $\times$ ) symbols denote  $N = 20$ , refinement level  $n_{\text{ref}} = 1$  and refinement ratio  $R_{\text{ref}}^1 = 4$ . The square ( $\square$ ) symbols denote  $N = 20$ ,  $n_{\text{ref}} = 2$ ,  $R_{\text{ref}}^1 = R_{\text{ref}}^2 = 4$ . The triangle ( $\nabla$ ) symbols denote  $N = 20$ ,  $n_{\text{ref}} = 3$ ,  $R_{\text{ref}}^1 = R_{\text{ref}}^2 = R_{\text{ref}}^3 = 4$ . The circle ( $\circ$ ) symbols denote  $N = 20$ ,  $n_{\text{ref}} = 5$ ,  $R_{\text{ref}}^1 = R_{\text{ref}}^2 = R_{\text{ref}}^3 = 4$  and  $R_{\text{ref}}^4 = 2$ .



358

359 Fig. S3. (a)-(e) Spatial distribution of the instantaneous feeding current without the presence of  
 360 the prey,  $\mathbf{u}(\mathbf{x},t)$ , in a plane coincident with the centerlines of the antennules (A1) at 5 selected  
 361 time frames during the hundredth beating cycle ( $N = 99$ ). The maximum  $|\mathbf{u}(\mathbf{x},t)|$  is limited to 5  
 362 mm/s to show the flow pattern around A1. In each panel, the pseudocolor plot shows the  
 363 magnitude of the feeding current, while the arrows show the direction of the feeding current  
 364 projected to the visualization plane. The whitest zones indicate the area occupied by A1 and  
 365 copepod body, while the darkest zones represent the flow around the feeding appendages.



366

367 Fig. S4. (a) Spatial distributions of the feeding current without the presence of the prey averaged

368 over one beating cycle,  $\mathbf{u}_{\text{avg}}$ , in a plane coincident with the centerlines of the antennules (A1).

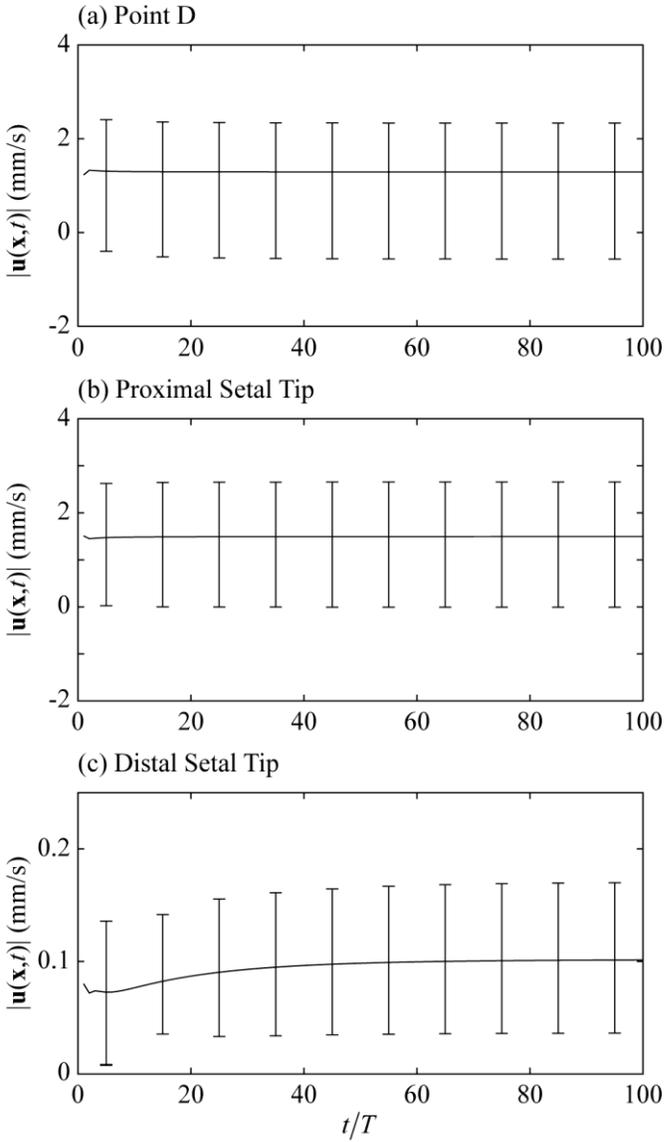
369 The pseudocolor plot shows the magnitude of the feeding current, while the arrows show the

370 direction of the feeding current projected to the visualization plane. (b) Pseudocolor plot of the

371 peak-to-peak magnitude of the oscillatory component of the feeding current without the presence

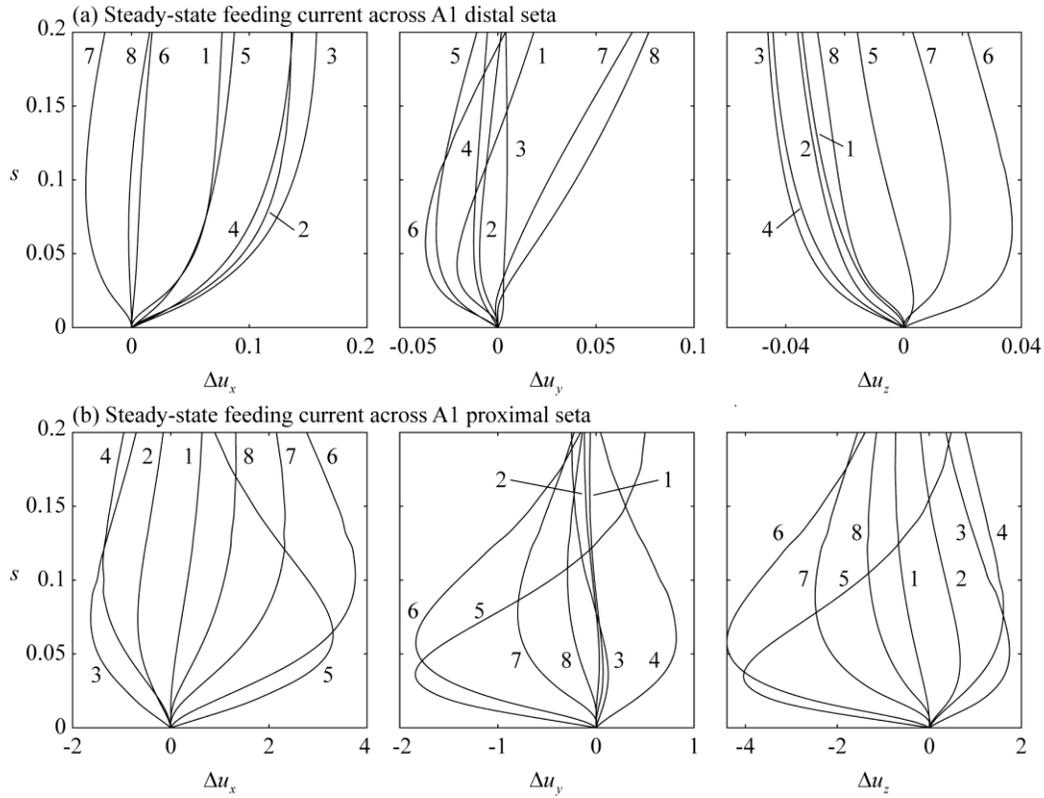
372 of the prey in a plane coincident with the A1 centerlines. The maximum magnitudes in panels (a)

373 and (b) are limited to 1.8 mm/s and 10 mm/s, respectively, to show the corresponding flow  
374 pattern around A1.



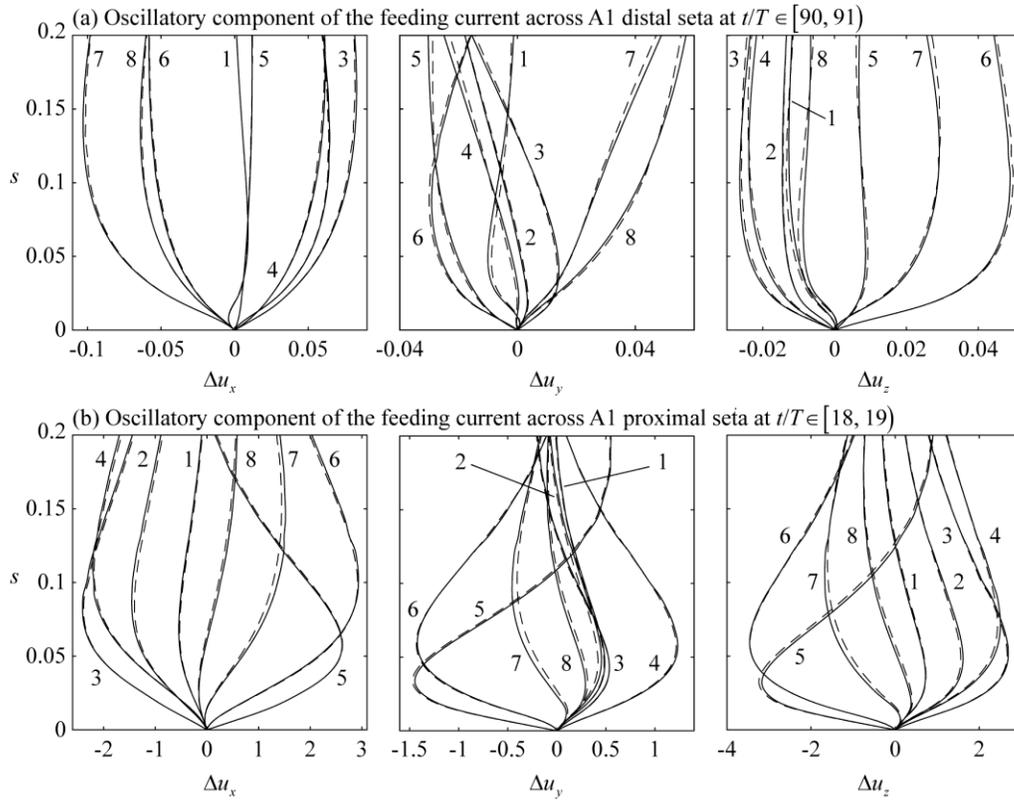
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376 Fig. S5. Magnitude of the feeding current without the presence of the prey,  $|\mathbf{u}(\mathbf{x},t)|$ , at (a) Point D,  
 377 the tips of the (b) proximal and (c) distal setae on the antennule as a function of beating cycle.  
 378 The copepod's feeding appendages are beating at 30 Hz. The solid line in each panel represents  
 379 the feeding current averaged over one beating cycle, while vertical bars represent the range of the  
 380 oscillatory component of the feeding current at the selected beating cycles.



381

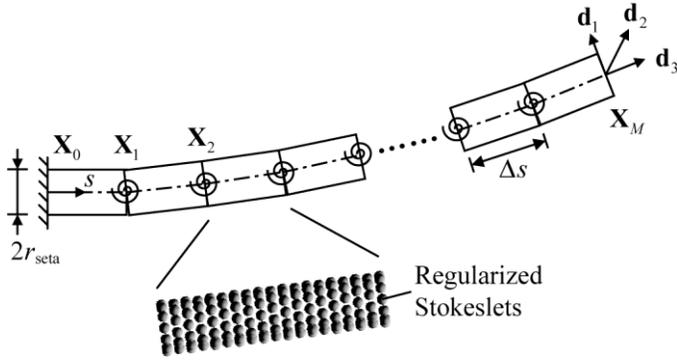
382 Fig. S6. Instantaneous bending flow,  $\Delta \mathbf{u}(s,t)$ , across the left (a) distal and (b) proximal setae on  
 383 the antennule without the presence of prey during one beating cycle, after the bending flow  
 384 averaged over one beating cycle reaches the steady state. A sequence of  $\Delta \mathbf{u}(s,t)$ , plotted in terms  
 385 of its components in the  $x$ ,  $y$  and  $z$  direction in units of mm/s, at equally spaced times during one  
 386 cycle of oscillation is labeled by the numbers 1-8. The arclength along the setal centerline ( $s$ ,  
 387 units of mm) is measured starting at the setal root.



388

389 Fig. S7. Oscillatory components of the bending flows,  $\Delta \mathbf{u}_{\text{osc}}(s,t)$ , across the left (a) distal and (b)  
 390 proximal setae on the antennule in the beating cycle during which the time-averaged bending  
 391 flow induced by the free-floating prey is the largest across the corresponding seta. A sequence of  
 392 shapes  $\Delta \mathbf{u}_{\text{osc}}(s,t)$ , plotted in terms of its components in the  $x$ ,  $y$  and  $z$  direction in units of mm/s, at  
 393 equally spaced times during the beating cycle is labeled by the numbers 1-8. The arclength along  
 394 the setal centerline ( $s$ , units of mm) is measured starting at the setal root.

395



396

397 Fig. S8. Schematic of the clamped seta in our numerical model. The arclength of the seta is  $L_{\text{seta}}$ ,  
 398 and radius  $r_{\text{seta}}$ . The Lagrangian parameter  $s \in [0, L_{\text{seta}}]$  is defined to start from the setal root and  
 399 along the setal centerline. The three orthogonal vectors,  $\mathbf{d}_1$ ,  $\mathbf{d}_2$  and  $\mathbf{d}_3$ , are to represent the setal  
 400 orientation, with  $\mathbf{d}_3$  along the  $s$  direction. The seta is discretized into  $M$  segments of equal arc  
 401 length  $\Delta s$ . The physical centerline coordinates of the two  $m$ -th segment nodes are represented by  
 402  $\mathbf{X}_m$  and  $\mathbf{X}_{m+1}$ , for  $m = 0, 1, \dots, M - 1$ . The regularized Stokeslets are distributed uniformly at the  
 403 surface of each segment.