<table>
<thead>
<tr>
<th><strong>Title</strong></th>
<th>Magnetic field enriched surface enhanced resonance Raman spectroscopy for early malaria diagnosis</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Author(s)</strong></td>
<td>Yuen, Clement; Liu, Quan</td>
</tr>
<tr>
<td><strong>Citation</strong></td>
<td>Yuen, C., &amp; Liu, Q. (2012). Magnetic field enriched surface enhanced resonance Raman spectroscopy for early malaria diagnosis. Journal of Biomedical Optics, 17(1), 017005.</td>
</tr>
<tr>
<td><strong>Date</strong></td>
<td>2012</td>
</tr>
<tr>
<td><strong>URL</strong></td>
<td><a href="http://hdl.handle.net/10220/10201">http://hdl.handle.net/10220/10201</a></td>
</tr>
<tr>
<td><strong>Rights</strong></td>
<td>© 2012 Society of Photo-Optical Instrumentation Engineers. This paper was published in Journal of Biomedical Optics and is made available as an electronic reprint (preprint) with permission of Society of Photo-Optical Instrumentation Engineers. The paper can be found at the following official DOI: [<a href="http://dx.doi.org/10.1117/1.JBO.17.1.017005">http://dx.doi.org/10.1117/1.JBO.17.1.017005</a>]. One print or electronic copy may be made for personal use only. Systematic or multiple reproduction, distribution to multiple locations via electronic or other means, duplication of any material in this paper for a fee or for commercial purposes, or modification of the content of the paper is prohibited and is subject to penalties under law.</td>
</tr>
</tbody>
</table>
Magnetic field enriched surface enhanced resonance Raman spectroscopy for early malaria diagnosis

Clement Yuen
Quan Liu
Magnetic field enriched surface enhanced resonance Raman spectroscopy for early malaria diagnosis

Clement Yuen and Quan Liu
Nanyang Technological University, Division of Bioengineering, School of Chemical and Biomedical Engineering, Singapore 637457

Abstract. Hemozoin is a by-product of malaria infection in erythrocytes, which has been explored as a biomarker for early malaria diagnosis. We report magnetic field-enriched surface-enhanced resonance Raman spectroscopy (SERRS) of \( \beta \)-hematin crystals, which are the equivalent of hemozoin biocrystals in spectroscopic features, by using magnetic nanoparticles with iron oxide core and silver shell (Fe\(_3\)O\(_4\)/Ag). The external magnetic field enriches \( \beta \)-hematin crystals and enhances the binding between \( \beta \)-hematin crystals and magnetic nanoparticles, which provides further improvement in SERRS signals. The magnetic field-enriched SERRS signal of \( \beta \)-hematin crystals shows five orders of magnitude enhancement in the Raman signal, and there is about three orders of magnitude improvement in the SERRS signal without the influence of magnetic field. The enhancement has led to a \( \beta \)-hematin detection limit at a concentration of 5 nM (roughly equivalent to 30 parasites/\( \mu \)l at the early stages of malaria infection), which demonstrates the potential of magnetic field-enriched SERRS technique in early malaria diagnosis. © 2012 Society of Photo-Optical Instrumentation Engineers (SPIE). [DOI: 10.1117/1.JBO.17.1.017005]

Keywords: hemozoin; Raman spectroscopy; surface-enhanced Raman scattering; resonance Raman; hematin; malaria.

PAPER 11464 received Aug. 27, 2011; revised manuscript received Nov. 18, 2011; accepted for publication Nov. 30, 2011; published online Feb. 7, 2012.

1 Introduction

Human malaria disease is a worldwide disease with estimated 225 million cases, accounting for 800,000 deaths per year. The disease is caused by a parasite protozoan, in which the parasite infects blood cells of the host and hemozoin biocrystals are disposed as byproducts after the ingestion of hemoglobins. Since the malaria disease can aggravate into a fatal illness within hours upon development of the first symptom, the early diagnosis of malaria infection is important, which requires the detection of hemozoin at low concentrations in infected blood cells. In malaria diagnosis, microscopic examination of blood smears remains the “gold standard” for the detection of malaria parasites, but this method is labor-intensive and time-consuming; moreover, special expertise from operators is required for reliable data interpretation. Therefore, the development of a sensitive technique, which requires minimal labor and expertise for hemozoin detection, is warranted in early malaria diagnosis.

Recently, several other malaria diagnosis techniques, such as the quantitative buffy coat method, the molecular diagnostic method, flow cytometry technique, serological tests, light scattering measurement, optical tweezing and laser desorption mass spectrometry, have been developed to overcome the shortcomings of the traditional method. Among these methods, resonance Raman spectroscopy (RRS) has been reported to amplify the Raman signal of hemozoin in malaria parasite-infected blood cells by the close Raman shift matching between the laser source and electronic transition of hemozoin. Moreover, surface-enhanced Raman scattering (SERS) effect has also been shown on a silver tip to enhance the Raman spectrum of hemozoin in infected cells via the augmented electromagnetic coupling between hematin and gold or silver nanoparticles.

The success in detecting the RRS and SERS signal of hemozoin shows the potential for further augmentation by combining the two effects, known as surface enhanced resonance Raman spectroscopy (SERRS). This SERRS technique has been demonstrated on other test molecules [rhodamine 6G (R6G)] adsorbed on silver nanoparticles for further enhancement in the Raman signal, as silver gives a higher enhancement than other metals (e.g., gold). The SERRS signal could be further enhanced by employing a magnetic field to enrich the hemozoin concentration. A similar strategy has been employed in other applications such as magnetic purification. Moreover, magnetic nanoparticles, e.g., nanoparticles made of iron oxide that show to be effective magnets at room temperature, could also attract and attach to hemozoin in a magnetic field because hemozoin is paramagnetic in nature, in a magnetic field. This approach is similar to the strategy reported for capturing and enriching bacteria.

In this work, we report a novel magnetic field enrichment strategy on SERRS by using magnetic nanoparticles to augment Raman signals from \( \beta \)-hematin crystals, similar to hemozoin in molecular, magnetic and Raman properties. The SERRS effect is further enhanced by the magnetic enrichment of \( \beta \)-hematin crystals and magnetic SERS-active nanoparticles with iron oxide core and silver shell. The performance of magnetic field-enriched SERRS quantified experimentally is compared with that of the SERRS without the influence of magnetic field, and the ordinary RRS on \( \beta \)-hematin crystals. Furthermore, the analytical enhancement factor and sensitivity of the proposed magnetic field-enriched SERRS technique are investigated.
2 Materials and Methods

2.1 Fabrication of Fe3O4@Ag Magnetic Nanoparticles

We synthesized the nanoparticles with iron oxide core and silver shell by using the seed-growth reduction method. First, a total of 16.2 mM Fe3O4 nanoparticles (Iron II, III oxide nanopowder, Sigma-Aldrich, USA) in ethanol (20 ml) was added drop-wise to 80 ml of ethanol with 0.15 g of polycrylic acid (Potassium polyacrylate, Sigma-Aldrich, USA). Then the mixture was sonicated (Elma E30H, Elma, Switzerland) for 15 min. The Fe3O4 nanoparticles were separated with a magnet and washed with ethanol. The separated Fe3O4 nanoparticles were re-dispersed (2.1 mM) in a mixture of ethanol and deionized water sequentially, then filtered and collected with 0.2 μm supor filters. The resulting nanoparticles were suspended in 15 ml methanol and then filtered with 0.2 μm supor filters (0.2 μm supor syringe filters, Pall, USA).

2.2 Synthesis of β-Hematin Crystals

β-hematin crystals were fabricated using an acid-catalyzed method. A 0.1 M NaOH solution diluted with 7.9 mM of Ferriporphyrin IX chloride [C1-Fe(III)PPIX, hemat chloride, MP Biomedicals, USA] was heated at 60°C and stirred at 150 rpm. 1.45 ml of HCl (1 M) and 8.825 ml of acetate solution were added to the mixture, after 10 min and 14 min, respectively. After another 46 min, the heater was removed and the mixture was left undisturbed in a dark environment for 24 h. The solute was washed with methanol and deionized water sequentially, then filtered and collected with 0.2 μm supor filters for drying at room temperature over P2O5 for 48 h. The dry β-hematin powder was resuspended by aqueous NaOH at concentrations ranging from 10^{-4} M to 10^{-11} M to obtain β-hematin suspension at concentrations ranging from 1 × 10^{-2} M to 1 × 10^{-9} M. NaOH was introduced to effectively disaggregate the large β-hematin particle into smaller crystals by breaking the interchain hydrogen bonds between β-hematin molecules. Due to the low concentration of NaOH used, the conversion of β-hematin to hematin was insignificant as compared to other studies in which NaOH at a much higher concentration was used. This ensured that measured Raman spectra were mainly contributed by β-hematin, which is confirmed by the characteristic peaks of β-hematin present in the spectra. To investigate the magnetic enrichment effect in smaller β-hematin, precipitate was disposed and supernatant was collected for Raman measurements from a β-hematin suspension (10^{-4} M) after centrifuging at 5000 rpm for 5 min (Sartorius 2-16, Sigma Laborzentrifugen, Germany).

2.3 Preparation of Analytes for Magnetic Field-enriched SERS Experiments

For the SERS measurements of R6G (Rhodamine 6G, Sigma-Aldrich, USA) absorbed on Fe3O4@Ag magnetic nanoparticles, R6G aqueous solutions were prepared at concentrations ranging from 10^{-6} to 10^{-8} M. As for the evaluation of SERS measurements of β-hematin crystals with and without magnetic field enrichment, the suspension of Fe3O4@Ag magnetic nanoparticles and β-hematin solution were each sonicated for 2 min. They were then mixed together (1:1 v/v) and underwent sonication for another 2 min. In all Raman measurements, the analyte was dropped inside a small vial made with aluminum foil for measurements, since aluminum has shown to give minimal background Raman signal within the spectral region of interest in this study. The small vial was placed on top of a magnet, around which the magnetic field was 0.198 T and the magnetic field gradient was 26.6 T/m, during the SERS and RRS measurements with magnetic field enrichment.

2.4 Field Emission Scanning Electron Microscope and Transmission Electron Microscope with Energy-dispersive X-rays Analysis

For taking field emission scanning electron microscopy (FESEM) images, a thin layer of platinum was coated with a fine coater (JEOL JFC-1600, JEOL, Japan) at 20 mA for 80 s on the sample surface prior to the FESEM (JEOL JSM-6700F, JEOL, Japan) examination of Fe3O4@Ag magnetic nanoparticles. The sample was prepared by drying nanoparticle suspension that was dropped onto a copper TEM grid (300 mesh holey-carbon copper TEM grid, Ted Pella, USA) prior to image acquisition.

2.5 Raman Instrumentation

We evaluated the SERS signals of R6G, and investigated the SERS and RRS properties of β-hematin crystals with and without magnetic field using a micro-Raman spectrometer system (inVia, Renishaw, UK) coupled with a microscope (Alpha 300, WITec, Germany) in a backscattering geometry. A 633 nm laser (Renishaw, UK) beam, reported to be feasible for inducing SERS effect on Ag, was focused onto the samples at a spot size of about 3 μm through a microscope objective (20×, N.A. 0.4, Leica). The excitation power was 0.1 mW for all SERS and SERRS measurement, which is typically used in literature to avoid localized heating. For the ordinary Raman experiment, a signal-to-noise ratio, S/N, of about 5 was required in all Raman spectra for the determination of minimum detectable concentrations of R6G and β-hematin, where N was the average noise intensity in the spectral region next to a representative Raman peak (1000 cm^{-1} for R6G and at 1750 cm^{-1} for β-hematin), and S was the difference between the peak intensity (1635 cm^{-1} for R6G and 1628 cm^{-1} for β-hematin).
for β-hematin) and the average noise intensity. All Raman spectra were collected with an exposure time of 15 s, and averaged from more than five different locations with a standard deviation of less than 5% for R6G, and of less than 10% for β-hematin. In each raw spectrum, a fifth-order polynomial was found to be optimal for fitting the fluorescence background, in which this polynomial was subtracted from the raw spectrum to yield the final spectrum.25

3 Results

Figure 1(a) gives the FESEM image of the raw Fe3O4 nanoparticles. Individual Fe3O4 nanoparticles have a mean diameter of about 50 nm (±5 nm). Figure 1(b) shows the FESEM images of the Fe3O4 nanoparticles coated with silver shells. The Fe3O4@Ag nanoparticles were well dispersed in the image. Each Fe3O4@Ag nanoparticle has a mean diameter of about 140 nm [Fig. 1(c)], with a size range ±20 nm characterized by zetasizer measurements. The core-shell geometry is confirmed by the TEM image [Fig. 1(d)] with an EDX spectrum [Fig. 1(e)] that reveals the elemental composition of the nanoparticle. Fe, Ag, O, Cu and C can be observed in the EDX graph. Fe, O and Ag signals are originated from the Fe3O4 core and Ag shell, while Cu, O and C are attributed to surfactant. (Other structures in the image are attributed to surfactant). (e) EDX of the Fe3O4@Ag nanoparticles. (Fig. 1(e))

Figure 2 compares the SERS spectra of aqueous R6G solution [Fig. 2(a), concentrations varying from 10^-6 M to 10^-3 M] with the ordinary Raman spectra of R6G solution [Fig. 2(b), concentrations varying from 10^-2 M to 10^-1 M]. Most prominent Raman peaks, such as C─C─C ring in-plane bending (615 cm^-1), CH out-of-plane bending (775 cm^-1), C─O─C stretching (1185 cm^-1), C─C/C─N stretching (1310 cm^-1 and 1365 cm^-1), and aromatic C─C stretching (1508 cm^-1),26 can be observed in the SERS spectra of R6G. The minimum detectable concentration of R6G absorbed on the Fe3O4@Ag nanoparticles is 1 x 10^-8 M, which is five orders of magnitude more sensitive than that of 10^-3 M detected in the ordinary Raman spectrum without enhancement. We estimated27 that the analytical enhancement factor (AEF) of the SERS signals relative to the ordinary Raman measurement (AEF_{SERS/Raman,R6G}) is about 5.77 x 10^6, which is comparable to the AEF values (around 10^7 to 10^9) of nanoparticle colloids stated in the literature.27,28

These results suggested the feasibility of using the Fe3O4@Ag nanoparticles for enhancing the Raman signal of β-hematin crystals.

Figure 3 shows the FESEM image of β-hematin crystals fabricated using the acid-catalyzed method [Fig. 3(a) and 3(b)] and the size distribution of crystals [Fig. 3(c)]. The fabricated β-hematin crystals are comparable to the size of hemozoin biocrystals found in the ring stage parasites (estimated from the concentration per cell and density of hemozoin)29,30 that dominate over other stages32 in the bloodstream for detection. Close resemblance in the spatial dimensions between the two types of crystals presumably would result in similar SERRS enhancement effect. The minimization of fabricated hemozoin size is to avoid artificially higher enhancement in magnetic field enrichment since larger crystals will have higher magnetic field enrichment as shown in the result later. Hence, the acid-catalyzed method is preferred to fabricate smaller crystals over
...the anhydrously synthesized β-hematin or in the biochemically cloned hemozoin, although the resulted crystals may have lower crystallinity and smaller sizes as reported in Ref. 19.

Figure 4 compares resonance Raman spectra of hematin with [Fig. 4(a)–4(c)] and without [Fig. 4(d)–4(f)] magnetic field-enriched strategy at concentrations ranging from 10^{-3} M to 5 × 10^{-9} M. Prominent vibrational features, such as ν_{v2} (based on the electron spin and crystallographic coordination notation tetragonal D_{4h} system for resonance Raman peaks studies on myoglobin) at 345 cm^{-1}, ν_{v6} at 367 cm^{-1}, ν_{v15} at 754 cm^{-1}, ν_{v22} at 1120 cm^{-1}, ν_{v11} at 1551 cm^{-1}, ν_{v2} at 1570 cm^{-1}, and ν_{v10} at 1628 cm^{-1}, are noted in most of these spectra. The locations of these peaks are equal to those reported Raman peaks for hemozoin biocrystals, confirming that the spectral features of β-hematin crystals are equivalent to hemozoin in Raman spectroscopy. The effect of surface enhancement can be clearly distinguished when the SERRS [Fig. 4(a) and 4(d)] are compared with the RRS measurements [Fig. 4(b) and 4(e)] and the RRS measurements by using Fe_{3}O_{4} nanoparticles [Fig. 4(c) and 4(f)]. We also note that the lowest detectable concentrations of β-hematin for SERRS with Fe_{3}O_{4}@Ag nanoparticles, RRS, and RRS with Fe_{3}O_{4} nanoparticles under magnetic field enrichment are 5 × 10^{-9} M, 5 × 10^{-7} M, and 5 × 10^{-7} M, respectively, and those without magnetic field enrichment are 5 × 10^{-6} M, 5 × 10^{-4} M, and 5 × 10^{-4} M, respectively, where the excitation power in the SERRS measurements was 0.1 mW and that in the RRS measurements was 10 mW.

4 Discussion
We have demonstrated the feasibility and significant improvement of magnetic field-enriched SERRS over conventional SERRS for detecting β-hematin crystals at low concentrations. To gain additional insight into Raman enhancement in this technique, we calculated the analytical enhancement factor (AEF) in each of the following techniques relative to the RRS measurement of β-hematin crystals without Fe_{3}O_{4} nanoparticles [Fig. 4(e)]:
1. magnetic field-enriched SERRS (AEF_{magSERRS/RRS,β-hema}),
2. SERRS without magnetic field (AEF_{SERRS/RRS,β-hema}), and
3. magnetic field-enriched RRS (AEF_{magRRS/RRS,β-hema}). These AEFs have been calculated by applying Eq. (1):

\[
AEF = \left( \frac{I_{1628,\text{Augmented}}}{I_{1628,\text{Ref}}} \right) \times \left( \frac{C_{\text{Ref}}}{C_{\text{Augmented}}} \right),
\]

where \(I_{1628,\text{Augmented}}/I_{1628,\text{Ref}}\), and \(C_{\text{Augmented}}/C_{\text{Ref}}\) are the ratio of Raman intensity at 1628 cm^{-1}, and the ratio of β-hematin concentration, respectively, in the measurements to be evaluated (magnetic field-enriched SERRS, SERRS, or magnetic field-enriched RRS) to those in the reference measurement (RRS). The estimated AEF values are listed as follows: AEF_{magSERRS/RRS,β-hema} ≈ 2.30 × 10^{3}, AEF_{SERRS/RRS,β-hema} ≈ 1.54 × 10^{3}, and AEF_{magRRS/RRS,β-hema} ≈ 68. Hence, the magnetic field enrichment can improve the signal intensities by roughly two orders of magnitude. The three orders of magnitude augmentation in the detection limit between the measurements with and without the magnetic field enriched can be attributed to the reduced noise level in the Raman signal in the magnetic field-enriched measurement.

The enhancement mechanism behind the addition of Fe_{3}O_{4}@Ag nanoparticles is studied. SERRS signal of β-hematin [Fig. 4(d)] is only exhibited by mixing nanoparticles with the SERS-active silver shell and β-hematin. RRS is resulted for Fe_{3}O_{4} nanoparticles and β-hematin mixture [Fig. 4(f)], with RRS signal comparable to that of β-hematin without any nanoparticles [Fig. 4(e)]. This observation also applies to the magnetic field-enriched measurement, with only SERRS enhancement noted in the mixture of Fe_{3}O_{4}@Ag nanoparticles and β-hematin [Fig. 4(a)], while RRS is exhibited in the β-hematin mixture with [Fig. 4(b)] and without [Fig. 4(c)] Fe_{3}O_{4} nanoparticles under a magnetic field. RRS intensities of β-hematin with Fe_{3}O_{4} nanoparticles under magnetic field is 1.4 times higher than that without Fe_{3}O_{4} nanoparticles, probably attributed to the enhanced aggregation of β-hematin due to the Fe_{3}O_{4} nanoparticles. The spectral shapes are similar in the SERRS and RRS spectra despite the fact that higher intensity is noted in the SERRS spectra. The similarity may be explained by the unchanged chemical structure and symmetry of β-hematin crystals that are magnetically held to the Fe_{3}O_{4}@Ag nanoparticles. Compared to many other molecules such as R6G, the adsorption of β-hematin crystals onto the Ag surface is weaker thus its SERRS spectrum is less influenced by the adsorption. The similar phenomenon is also observed in other chemicals that have weak interactions with Ag.

We have compared AEF_{SERRS/RRS} for β-hematin with AEF_{SERS/Raman} for R6G, since the two quantities are considered equivalent. The enhancement factor of SERS relative to...
ordinary Raman for R6G ($\text{AEF}_{\text{SERS}/\text{Raman}} \approx 5.77 \times 10^4$) is higher than that of the SERRS relative to RRS for $\beta$-hematin ($\text{AEF}_{\text{SERRS}/\text{RRS},\beta-\text{hema}} \approx 1.54 \times 10^5$), which can be attributed to the larger size of the $\beta$-hematin compared R6G molecules, with size (area) at least greater than roughly 30 nm x 30 nm (Fig. 3). Nevertheless, aggregates formed between magnetic $\beta$-hematin and the Fe$_3$O$_4$@Ag nanoparticles can still lead to effective SERS activities, similar to the configurations reported in the literature (e.g. localized AEF of about $10^5$ in configuration such as dimers and trimers). In addition, SERS can be observed in $\beta$-hematin at a distance from the Ag surface in the aggregation configuration (<40 nm), similar to that in other SERS nanoparticles. The AEF$_{\text{SERRS}/\text{RRS},\beta-\text{hema}}$ is compensated by the further augmentation in the magnetic field-enriched SERRS and RRS measurements, which can be explained by the following effects induced by the magnetic field. First, $\beta$-hematin is enriched. Second, more Fe$_3$O$_4$@Ag nanoparticles are attached to each $\beta$-hematin crystal and thus, leading to higher SERRS intensity. The potential mechanisms responsible for these effects are elaborated as follows.

The enrichment of $\beta$-hematin concentrations due to a magnetic field can be interpreted by the fact that paramagnetic $\beta$-hematin are attracted much faster to the bottom of the vial by the magnet than unmagnetized crystals without the influence of a magnetic field. Consequently, the concentration of $\beta$-hematin will be higher at the laser spot than that without the magnetic field, which has been demonstrated by a value of 68 in $\text{AEF}_{\text{magRRS}/\text{RRS},\beta-\text{hema}}$ for RRS measurements under the influence of a magnetic field in the absence of nanoparticles [Fig. 4(c)]. The magnetic field enrichment effect is more significant in larger $\beta$-hematin crystals, as confirmed by our Raman experiment in the $\beta$-hematin supernatant after centrifuging (Fig. 5). Higher $\text{AEF}_{\text{magRRS}/\text{RRS},\beta-\text{hema}}$ is observed in the magnetic field-enriched RRS for $\beta$-hematin mixture without centrifuging (68 in Fig. 4) than that calculated in the $\beta$-hematin supernatant (4 in Fig. 5). Hence, the magnetic field can effectively enrich $\beta$-hematin crystals to give rise to strong enhancement.

More nanoparticle-hematin aggregates are formed by an external magnetic field. Figure 6 shows that more Fe$_3$O$_4$@Ag nanoparticles are bound to $\beta$-hematin crystals in a magnetic field [Fig. 6(a)] compared to the case without a magnetic field [Fig. 6(b) and 6(c)]. Since the Fe$_3$O$_4$ core of the nanoparticles is ferromagnetic, the magnetic field produced by each Fe$_3$O$_4$@Ag nanoparticle attracts adjacent $\beta$-hematin crystals [Fig. 6(b) and 6(c)]. More Fe$_3$O$_4$@Ag nanoparticles are close or tightly bound to $\beta$-hematin crystals under an external magnetic field [Fig. 6(a)]. Figure 6(d) shows a schematic physical model for the configurations of Fe$_3$O$_4$@Ag nanoparticles and $\beta$-hematin crystals that leads to surface enhancement. For each crystal attached at the contact or in close vicinity (≤40 nm) in the gap to the Fe$_3$O$_4$@Ag nanoparticle, known as “hot spots,” intense SERS activities occur. Additional hot spots are formed with more aggregations with the application of an external magnetic field. The increased number of nanoparticles-hematin aggregates may be responsible for the further improvement in the $\text{AEF}_{\text{magSERRS}/\text{RRS},\beta-\text{hema}}$ in comparison with that in RRS without the involvement of nanoparticles as in $\text{AEF}_{\text{magRRS}/\text{RRS},\beta-\text{hema}}$ in Fig. 5. In contrast, the ratio of $\text{AEF}_{\text{magSERRS}/\text{RRS},\beta-\text{hema}}$ to $\text{AEF}_{\text{SERS}/\text{RRS},\beta-\text{hema}}$ in $\beta$-hematin supernatant (3540/1200 ≈ 3) is similar in magnitude to the $\text{AEF}_{\text{magRRS}/\text{RRS},\beta-\text{hema}}$, which is 19 [32] times larger than the $\text{AEF}_{\text{SERS}/\text{RRS},\beta-\text{hema}}$, in comparison with that in RRS without the involvement of nanoparticles as in $\text{AEF}_{\text{magRRS}/\text{RRS},\beta-\text{hema}}$ ≈ 68. In contrast, the ratio of $\text{EF}_{\text{magSERRS}/\text{RRS},\beta-\text{hema}}$ to $\text{EF}_{\text{SERRS}/\text{RRS},\beta-\text{hema}}$ in $\beta$-hematin supernatant (3540/1200 ≈ 3) is similar in magnitude to the $\text{AEF}_{\text{magRRS}/\text{RRS},\beta-\text{hema}}$, since the $\beta$-hematin supernatant contained mostly small crystals that are already attached on the nanoparticles. Therefore, more nanoparticle-hematin aggregates can give further augmentation in Raman signals, in addition to the SERRS and $\beta$-hematin enrichment effects.

With the two aforesaid magnetic field induced effects, we evaluate the detection limit of $\beta$-hematin using magnetic field-enriched SERRS by converting $\beta$-hematin concentration to the concentration of malaria parasites in blood for practical evaluation. The detection limit of $\beta$-hematin concentration at $5 \times 10^{-16}$ M in the magnetic field-enriched SERRS measurement obtained in this study is equivalent to roughly 30 parasites/µl (considering a hemozoin concentration of about 0.22 pg/cell in the earlier malaria infection at the ring stage and a molecular weight of 1229 g/mol for hemozoin) at the early stage. More importantly, the sensitivity is comparable to other rapid malaria detection techniques for hemozoin detection at later malaria stages, e.g. 10 parasites/µl (with hemozoin concentration at about 0.6 pg/cell). For laser desorption mass spectrometry and automated blood cell counters. With the high sensitivity in the detection of $\beta$-hematin in the current configuration
without optimization, the magnetic field-enhanced SERRS technique has demonstrated great potential for early malaria diagnosis. The detection sensitivity of our technique could be further improved by optimizing the configuration of the magnetic field and the physical geometry of SERS-active nanoparticles.

5 Conclusions

We report the detection of β-hematin crystals using magnetic field-enhanced SERRS enabled by Fe3O4@Ag nanoparticles. The method enriches β-hematin crystals and Fe3O4@Ag nanoparticles by applying an external magnetic field and synergizes with the enhancement capability of SERRS, thereby promoting further augmentation in the Raman signal of β-hematin crystals. A parasitemia level of 30 parasites/µl in blood in the early stages of infection can be achieved by using this method with the current setup, which demonstrates the potential of employing magnetic field-enhanced SERRS in early malaria diagnosis.

6 Appendix

6.1 Analytical Enhancement Factor Calculation

The analytical enhanced factors are calculated for the following. For rhodamine 6G (R6G) molecules, the SERS AEF of R6G molecules in the nanoparticles solution of iron oxide core coated with silver shell (Fe3O4@Ag) with respect to the ordinary Raman measurement (AEF_{SERS/Raman,R6G}) has been calculated. For the β-hematin crystals, 1. the equivalent magnetic field-enriched SERRS AEF (AEF_{magSERRS/RRS,β-hema}), 2. the SERRS AEF without magnetic field (AEF_{SERRS/RRS,β-hema}), and 3. the equivalent magnetic field-enriched RRS AEF (AEF_{magRRS/RRS,β-hema}) relative to RRS measurements have been calculated. The AEF in magnetic field-enriched measurement are equivalent AEF, in which the β-hematin concentrations are the concentrations prior to the magnetic field enrichment. These AEFs were calculated from the equation,

$$ AE F = \frac{I_{Augmented}}{I_{Ref}} \times \frac{P_{Augmented}}{P_{Ref}} \times \frac{C_{Ref}}{C_{Augmented}}, $$

where \( \frac{I_{Augmented}}{I_{Ref}} \), \( \frac{P_{Augmented}}{P_{Ref}} \) and \( \frac{C_{Augmented}}{C_{Ref}} \) are the ratios of the Raman intensities at Raman shift of \( \lambda \), excitation powers, and concentrations in enhanced and referenced measurements.

6.2 Calculation of AEF_{SERS/Raman,R6G}

The AEF_{SERS/Raman,R6G} of R6G in Fe3O4@Ag nanoparticle solution can be calculated as,

$$ AE F = \frac{I_{1365,Raman}}{I_{1365,Raman}} \times \frac{P_{Raman}}{P_{SERS}} \times \frac{C_{Raman}}{C_{SERS}} $n

$$ = \frac{9135.5 \times 10 mW}{1584 \times 0.1 mW} \times \frac{10^{-2} M}{10^{-6} M} \approx 5.77 \times 10^6, $$

where the two numbers 9135.5 and 1584 are the SERS and ordinary Raman intensities of R6G, respectively, at the concentrations of \( 10^{-6} M \) and \( 10^{-2} M \), excited at corresponding laser power of 0.1 mW and 10 mW (as in Fig. 2 in the main text).

6.3 Calculation of Equivalent AEF_{magSERRS/RRS,β−hema}, AEF_{SERRS/RRS,β−hema}, AEF_{magRRS/RRS,β−hema}

Similarly, the analytical enhancement factors in the measurement of magnetic field-enriched SERRS, SERRS and magnetic field-enriched RRS with reference to the RRS measurement of β-hematin crystals, can be calculated by Eq. (2). Table 1 gives the parameters for the calculation. Note that the equivalent AEFs are calculated in the magnetic field-enriched measurement, since the concentrations stated are concentrations of β-hematin prior to the use of a magnetic field. The AEF values are listed as follows: AEF_{magSERRS/RRS,β−hema} \( \approx 2.30 \times 10^6 \), AEF_{SERRS/RRS,β−hema} \( \approx 1.54 \times 10^5 \), and AEF_{magRRS/RRS,β−hema} \( \approx 68 \).

Table 1 Parameters used in the calculation of the AEF_{magSERRS/RRS,β-hema}, AEF_{SERRS/RRS,β-hema}, and AEF_{magRRS/RRS,β-hema} for β-hematin.

<table>
<thead>
<tr>
<th>Calculation of AEF_{magSERRS/RRS,β-hema}</th>
<th>I_{1628,Augmented} [a.u.]</th>
<th>I_{1628,Ref} [a.u.]</th>
<th>P_{Augmented} [mW]</th>
<th>P_{Ref} [mW]</th>
<th>C_{Augmented} [µM]</th>
<th>C_{Ref} [µM]</th>
<th>AEF</th>
</tr>
</thead>
<tbody>
<tr>
<td>Calculation of AEF_{SERRS/RRS,β-hema}</td>
<td>1494</td>
<td>1300</td>
<td>0.1</td>
<td>10</td>
<td>0.5</td>
<td>1</td>
<td>2.30 \times 10^6</td>
</tr>
<tr>
<td>Calculation of AEF_{magRRS/RRS,β-hema}</td>
<td>100</td>
<td>1300</td>
<td>0.1</td>
<td>10</td>
<td>5</td>
<td>1</td>
<td>1.54 \times 10^5</td>
</tr>
<tr>
<td>Calculation of AEF_{magRRS/RRS,β-hema}</td>
<td>442</td>
<td>1300</td>
<td>10</td>
<td>10</td>
<td>5</td>
<td>1</td>
<td>68</td>
</tr>
</tbody>
</table>

Table 2 Parameters used in the calculation of the AEF_{magSERRS/RRS,β-hema}, AEF_{SERRS/RRS,β-hema}, and AEF_{magRRS/RRS,β-hema} for β-hematin supernatant after centrifuging.

<table>
<thead>
<tr>
<th>Calculation of AEF_{magSERRS/RRS,β-hema}</th>
<th>I_{1628,Augmented} [a.u.]</th>
<th>I_{1628,Ref} [a.u.]</th>
<th>P_{Augmented} [mW]</th>
<th>P_{Ref} [mW]</th>
<th>AEF</th>
</tr>
</thead>
<tbody>
<tr>
<td>Calculation of AEF_{SERRS/RRS,β-hema}</td>
<td>20040</td>
<td>566</td>
<td>0.1</td>
<td>10</td>
<td>3.54 \times 10^5</td>
</tr>
<tr>
<td>Calculation of AEF_{magRRS/RRS,β-hema}</td>
<td>6768</td>
<td>566</td>
<td>0.1</td>
<td>10</td>
<td>1.20 \times 10^3</td>
</tr>
<tr>
<td>Calculation of AEF_{magRRS/RRS,β-hema}</td>
<td>2264</td>
<td>566</td>
<td>10</td>
<td>10</td>
<td>4</td>
</tr>
</tbody>
</table>

Journal of Biomedical Optics 017005-6 January 2012 • Vol. 17(1)
Table 2 gives the parameters for the calculation of the analytical enhancement factors in the measurement of magnetic field-enriched SERRS, SERRS and magnetic field-enriched RRS with reference to the RRS measurement of β-hematin supernatant after centrifuging. The results are $AEF_{magSERRS/RRS,β-hema} \approx 3.54 \times 10^3$, $AEF_{SERRS/RRS,β-hema} \approx 1.20 \times 10^3$, and $AEF_{magRRS/RRS,β-hema} \approx 4$.

Acknowledgments

This research was funded by the Bill and Melinda Gates Foundation through the Grand Challenges Explorations Initiative (Grant No. OPP1015169).

References